

Classification of Mild Cognitive Impairment Subtypes using Neuropsychological Data

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Abstract: While the research on Alzheimer's disease (AD) is progressing, timely intervention before an individual becomes demented is often emphasized. Mild Cognitive Impairment (MCI), which is thought of as a prodromal syndrome to AD, may be useful in this context as potential interventions can be applied to individuals at increased risk of developing dementia. The current study attempts to address this problem using a selection of machine learning algorithms to discriminate between cognitively normal individuals and MCI individuals among a cohort of community dwelling individuals aged 70-90 years based on neuropsychological test performance. The overall best algorithm in our experiments was AdaBoost with decision trees while random forests was consistently stable. Ten-fold cross validation was used with ten repetitions to reduce variability and assess generalizing capabilities of the trained models. The results presented are consistently of the same calibre or better than the limited number of similar studies reported in the literature.

1 INTRODUCTION

Decline in cognitive functions including memory, processing speed and executive processes has been associated with aging for sometime (Hedden and Gabrieli, 2004). It is understood that every human will go through this process, but some will go through it faster and for some, this process starts earlier (Chua et al., 2009; Cui et al., 2012a; Gauthier et al., 2006). Differentiating between cognitive decline due to a pathological process from normal aging is an ongoing research challenge. One of the best studied diseases in this context is Alzheimer's disease (AD), which is a neurodegenerative disease that can cause progressive cognitive impairment with devastating effects for the patients and their families. Although a cure for AD has not been found yet, it is often stressed that early identification of individuals at risk of AD can be instrumental in treatment and management.

Mild Cognitive Impairment (MCI) is considered a prodromal stage to dementia and may reflect the early clinical symptoms of a neurodegenerative disease such as AD (Chételat et al., 2005; Cui et al., 2012b; Haller et al., 2013; Petersen et al., 2009).

Patients with MCI have a higher probability of progressing to certain types of dementia, the most common being AD. Epidemiological studies suggest that the progression rate from MCI to dementia is around 10-12% annually (Mitchell and Shiri-Feshki, 2009). Therefore, accurate and early diagnosis of MCI is often stressed, as those patients can be closely monitored for progression to AD. While there are accepted consensus diagnostic criteria for MCI (Winblad et al., 2004; Albert et al., 2011), how each of these criteria is operationalized is less clear, resulting in differing rates of MCI across studies and regions (Kochan et al., 2010). In turn, this makes it difficult to predict progression to AD as well. Researchers usually focus on three distinct yet related problems in this area: (i) differentiating between cognitively normal (CN) and MCI individuals, (ii) predicting conversion from MCI to AD and (iii) predicting the time to conversion from MCI to AD (Lemos et al., 2012). We focus on the first problem in this paper.

There is also an interest in identifying subtypes of MCI, because each subtype is related to specific types of dementia and differential rates of conversion to dementia. Therefore, we also focus on MCI sub-

Table 1: The subtypes of MCI.

Amnestic subtype of MCI (aMCI)	Non-amnestic subtype of MCI (naMCI)
Single domain aMCI (sd-aMCI)	Single domain naMCI (sd-naMCI)
Multi domain aMCI (md-aMCI)	Multi domain naMCI (md-naMCI)

type classification.

There are two major subtypes of MCI; amnestic subtype of MCI and non-amnestic subtype of MCI. Amnestic subtype of MCI (aMCI) refers to impairment in memory, while non-amnestic subtype of MCI (naMCI) refers to non-memory impairments affecting executive functions, attention, visuospatial ability or language. These two subtypes are further divided depending on the number of domains impaired. Thus, we end up with four subtypes of MCI as seen in Table 1 (Winblad et al., 2004; Albert et al., 2011): Recent studies point out that md-aMCI has the highest probability of progress to AD and to dementia (Ganguli et al., 2011). Previous work in this area has focused on studying different modalities of Magnetic Resonance (MR) images in order to differentiate between different subtypes of MCI (Alexander et al., 2007; Chételat et al., 2005; Chua et al., 2008; Chua et al., 2009; Haller et al., 2013; Hinrichs et al., 2011; Reddy et al., 2013; Raamana et al., 2014; Reppermund et al., 2014; Sachdev et al., 2013b; Sachdev et al., 2013a; Thillainadesan et al., 2012). While several studies have shown that MR images, especially diffusion tensor imaging, can accurately portray micro-structural changes indicating neurodegenerative disease, the performance of the models could be improved. We focus on the neuropsychological test scores first and plan to integrate image based features at a later stage. In this study, we present the first in-depth assessment of neuropsychological measures (NM) in differentiating between MCI with its subtypes and CN individuals. A degree of circularity appears to be involved when using neuropsychological measures which we elaborate in the discussion section.

The remainder of this paper is organized as follows. The materials and datasets used are described in section 2. We then introduce the methods, pivoting on the core machine learning concepts used. The results of our study are in section 3 and we conclude this study in the final section with a discussion on results and indicating future directions of research.

Table 2: Demographic characteristics of the participants at baseline.

Sample size: 837	Baseline (wave 1)
Age (years)	78.57 \pm 4.51 (70.29-90.67)
Sex (male/female)	43.07% / 56.92%
Education (years)	12.00 \pm 3.65
MMSE (Mini-Mental State Exam)	28.77 \pm 1.26
CDR (Clinical Dementia Rating)	0.066 \pm 0.169

2 MATERIALS AND METHODS

2.1 Participants

The dataset we use was drawn from the Sydney Memory and Aging Study (MAS) that comprised 1037 community-dwelling, non-demented individuals recruited randomly through electoral rolls from two electorates of East Sydney, Australia (Sachdev et al., 2010). These individuals were aged 70-90 years old at the baseline. Each participant was administered a comprehensive neuropsychological test battery, and 52% underwent an MRI scan. Individuals were excluded if they had a Mini-Mental State Examination (MMSE) score $<$ 24 (adjusted for age, years of education and non-English-speaking background), a diagnosis of dementia, mental retardation, psychotic disorder (including schizophrenia and bipolar disorder), multiple sclerosis, motor neuron disease and progressive malignancy or inadequate English to complete assessments. Three repetitive waves after the baseline assessment have been carried out to date at a frequency of 2 years. Details of the sampling methodology have been published previously (Sachdev et al., 2010). This study was approved by the Human Research Ethics Committees of the University of New South Wales and the South Eastern Sydney and Illawarra Area Health Service, and all participants gave written informed consent. The demographics of the participants at baseline are given in Table 2. Only non-demented individuals from English speaking backgrounds with complete neuropsychological measures available were selected for the study.

2.2 Cognitive Assessments

A selection of available clinical and neuropsychological data was used by an algorithm to diagnose MCI in accordance with international criteria (Winblad et al.,

2004; Sachdev et al., 2010): (i) complaint of decline in memory and/or other cognitive functions by the participant or knowledgeable informant; (ii) preserved instrumental activities of daily living (Bayer ADL Scale (Hindmarch et al., 1998) score < 3.0); (iii) objectively assessed cognitive impairment (any neuropsychological test score ≥ 1.5 standard deviations (SDs) below published norms), (iv) not demented. Individuals are considered cognitively normal (CN) when performance on all measures were above the 7th percentile (≥ 1.5 SD) compared to published normative data, adjusted for age and education where possible. Over and above this procedure, at each wave, cases were brought to a panel of old age psychiatrists, neuropsychiatrists and neuropsychologists when there were unusual clinical features or an indication that an individual may have dementia. Consensus diagnosis of MCI, dementia or cognitively normal was made using all available data including clinical history, neuropsychological performance and MRI scans where available. Detailed methodology can be found (Sachdev et al., 2010).

The neuropsychological tests administered at baseline have been previously described (Sachdev et al., 2010). Thirteen measures from 11 standardised psychometric tests were administered by trained research psychologists measuring premorbid IQ, attention/information processing speed, motor speed, memory, language, visuo-spatial and executive abilities. We examine the raw versions of these scores rather than the age, sex and education adjusted scores, as this preprocessing step can result in improper model selection and overoptimistic results (Lemm et al., 2011).

The tests were administered over the next three waves at follow up intervals of two years each. When the expert panel were consulted, they examined all available data before coming up with a diagnosis, including the neuropsychological measures as well as MRI scans where available.

2.3 Classification using Neuropsychological Test Scores

We used the neuropsychological test scores described in the subsection 2.2 to train models that differentiate between classes. The consensus diagnosis is treated as a sample label. The algorithms used are all supervised learning algorithms as we have labeled data. We trained supervised binary classifiers using different algorithms. These experiments were performed using four different algorithms, which are described next. We then elaborate on the experimental setup used and the subclasses for classification.

2.3.1 Support Vector Machine

Support vector machines (SVM) can be considered as a more recent algorithm compared to the history of other learning algorithms (Cortes and Vapnik, 1995). SVM is a margin based technique, where the margin on either side of a hyperplane that separates two data classes is maximized. This creates the largest possible distance between the separating hyperplane and the instances on either side of it have been proven to reduce an upper bound on the expected generalization error. A better description of SVMs can be found (Maglogiannis, 2007; Crisci et al., 2012; Kotsiantis, 2007). A grid search with cross validation was used to find the optimum parameters for the SVM.

2.3.2 Random Forest

This method is based on decision trees which is one of the oldest techniques used for classification and has evolved much in the last two decades. A good overview can be found (Murthy, 1998). Decision trees can be considered as trees that classify instances by sorting based on feature values (Maglogiannis, 2007). Each node in a decision tree represents a feature of an instance to be classified and each branch represents a value that the node can take. The classification of instances starts from the root node and instances are sorted based on their feature values.

A random forest (RF) is a collection of decision trees (Liaw and Wiener, 2002). Classification for a new instance is obtained by majority vote over the classifications provided by individual trees included in the forest. A random bootstrap sample of data is used to train a tree which adds an additional layer of randomness to bagging (Liaw and Wiener, 2002). Conventional decision trees use the best split among all variables to decide how each node is split. However, best split among a subset of all variables is chosen in random forest. Although this may appear counterintuitive, it has been pointed that random forests perform comparably or better than a majority of classifiers such as discriminant analysis, SVM and neural networks, and are also inherently robust against overfitting.

2.3.3 AdaBoost

AdaBoost (AB) is a variant of boosting (Freund and Schapire, 1999). The roots of boosting go back as far as the theoretical framework of PAC (Probably Approximately Correct) learning. It builds on the concept that a 'weak' learning algorithm that performs slightly better than chance (random guessing) can be boosted into a strong learning algorithm. AdaBoost is

a variant of boosting that addresses the potential difficulties faced by other boosting algorithms and has become a standard in recent times.

The AdaBoost algorithm description is available (Freund and Schapire, 1999). We use decision trees as the base algorithm for AdaBoost.

2.3.4 Ensemble Methods

The underlying concept of ensemble methods (ES) is similar to boosting. A set of weak learners that performs slightly better than chance can be integrated to train a strong classifier. While many other methods of integration exist, we focus on weighted averaging and voting. The usual variants are bagging and boosting when the algorithm only uses one type of base learner. The ensemble method we use is trained with multiple types of base learners and is integrated using voting. Multiple versions of base learners are trained with varying parameters and the best classifiers are determined. While some classifiers can be considered as the best reported, others yield mediocre performance. Therefore, instead of combining the good and bad models together, a forward stepwise selection is used to select the subset of models that when averaged together yields excellent performance.

We use five types of base learners: SVM, k-nearest neighbour, decision trees, REPTree and random forest. A detailed description of the underlying ensemble selection method can be found (Caruana et al., 2004). It should be noted that random forest is also type of an ensemble method, however, we refer to the procedure described above as ensemble method for the rest of this paper.

2.3.5 Experimental Setup

We use Weka experimenter (v3.7) to carry out the experiments (Hall et al., 2009). All experiments utilize ten-fold cross validation with ten repetitions to eliminate bias and improve the reliability of the results. The different class labels used are tabulated in Table 3. While the first column resembles conventional machine learning experiments, the second column specifies the use of one class as positive and everything else as negative instances. For example, in aMCI against CN, the positive class is aMCI while CN is the negative class. Individuals with naMCI are not used to train this classifier. In contrast, aMCI against everything else uses aMCI as the positive class and everything else as the negative class which includes naMCI as well. While this increases class imbalance, we believe the increased number of negative instances together with the careful selection of

algorithms, leads to performance improvement as evidenced by the results.

Table 3: The different classes used for experimentation.

One vs One	One vs All
MCI — CN	aMCI — everything else
aMCI — CN	naMCI — everything else
naMCI — CN	sd-naMCI — everything else
aMCI — naMCI	md-naMCI — everything else
sd-aMCI — md-aMCI	sd-aMCI — everything else
sd-naMCI — md-naMCI	md-aMCI — everything else

We also carry out feature subset selection in order to reduce the feature space and improve the performance. We experiment with three types of feature subset selection methods including similarity based feature selection, information gain based feature selection, wrapper based feature selection, and present our observations.

As earlier described, the dataset was acquired in four individual waves and we treat them as four separate datasets. We execute the denoted experiments over the four waves separately and present the results. In fact, this constitutes one of the largest datasets reported in the literature as our sample from the first wave has 837 patients altogether, of which 505 are CN individuals and 332 are MCI individuals. Although the numbers decrease as the waves progress, the varying levels of progression warrants consideration of the four waves as four different and distinct datasets and demonstrates the validity of our results. We used 35 features to train the classifiers for the first wave while 29, 28 and 28 features were used to train classifiers for the second, third and fourth waves respectively.

3 RESULTS

The results of the experiments are presented in two main subsections. The first subsection discusses the results obtained from training binary classifiers of one vs one classes, while the second subsection discusses the results obtained from training binary classifiers of one vs all classes.

3.1 One vs One Classes

We present the performance of models trained over the first wave in Figure 1. While four algorithms were used for comparison, we only present the results of the best three algorithms for clarity. As can

be seen, AdaBoost and Ensemble Selection have performed very well on this dataset and random forest follows closely. We are unable to draw a direct comparison, as we could not find studies that used the same neuropsychological tests as ours. We report on the closest studies we can find (Lemos et al., 2012; Cui et al., 2012a). Lemos et al. report the classification results on differentiating MCI from AD, whereas Cui et al. report the classification results of predicting progression to MCI from CN. The best performance reported by the first work is an accuracy of 82% with a sensitivity of 76% and specificity of 83% while the second work noted that their best performance is an accuracy of 78.51% with an AUC of 0.841. Although the results we report do not constitute a direct comparison, they are consistently of the same calibre or better than those reported by these studies. In addition, we also compare our results to the best results reported by Reddy et al. who used the same dataset as ours. Their study used a derived set of features from the MRI based features, in order to differentiate between subtypes of aMCI. While they report an accuracy of 0.58 with an AUC of 0.67 in classifying sd-aMCI and md-aMCI, our model exhibits an accuracy of 0.847 with an AUC of 0.88 which is a significant improvement over the reported results.

We then proceed to add further validation to the performance of the trained models by repeating the same experiments over the next three waves as well. In the interests of clarity, we only include the best performing classifier for each classification experiment for each wave, which are plotted in Figure 2. It should be noted that, while in some cases, the best performing algorithm is unanimous, other cases exhibit differences in performance metrics. For example, in naMCI subtype classification of the second wave, while AdaBoost outperforms random forest in accuracy (85.14% to 82.47%), random forest significantly outperforms AdaBoost in AUC measure (0.68 to 0.86). In such cases, we consider random forest as the better performer.

We tried a range of feature selection algorithms in order to assess the effect on final classification performance of the models. We chose a relatively stable algorithm, namely random forest, to assess the impact of feature selection. Three major categories of feature selection algorithms were used: correlation based feature selection, information gain based feature selection and wrapper based feature selection. Specific algorithms used are (i) Correlation based subset evaluation (ii) Pearson correlation based (iii) Cross validation based (iv) Gain ratio based (v) Information gain based (vi) SVM wrapper based (vii) Random forest wrapper based and (viii) RELIEFF. More about these

algorithms can be found (Hall et al., 2009). Only one model was significantly improved by feature subset selection, namely the classification of MCI subtypes where the accuracy was improved to 91.27% from 86.01%. In presenting the results of feature selection, we opted not to include any method that does not improve the accuracy of at least three classifiers out of the six being tested. Only two methods remained and the difference in accuracy and AUC of these two methods are shown in Figure 3.

As can be interpreted from the results, feature subset selection did not improve the performance of the classifiers significantly and therefore, we refrained from further use of feature selection in this work.

3.2 One vs All Classes

The performance of the models trained on one vs all classes of the first wave is shown in Figure 4. Clearly the accuracy of the trained models has improved significantly in most cases. However, the AUC has typically decreased compared to the one vs one class scenario. This phenomenon can be explained when sample size is taken into consideration. For example, considering naMCI vs everything else, it can be seen that the ratio of positive to negative class is 1:4.6 which helps to improve the accuracy. The same reason causes the decrease in AUC, as specificity is increased and sensitivity is decreased.

For the sake of clarity, the results of the next three waves are represented in a plot where we only consider the best classifier, as shown in Figure 5. In selecting the best classifier, we thresholded the minimum AUC to 0.85 and ordered the results using accuracy. While AdaBoost still scores highest in accuracy in most cases, random forest turns out to be a better one vs all classifier in terms of AUC.

The intention behind developing one vs all classifiers is to come up with a multi-class classifier that can be used to classify a general population into CN, MCI and its subtypes where applicable. Our study is the first time that such an attempt has been made.

4 DISCUSSION

This study was devised to investigate the diagnostic value of neuropsychological features alone in differentiating MCI and its subtypes. We trained multiple classifiers including MCI versus CN, and differentiating between subtypes of aMCI and naMCI. This level of detail is warranted as it has been shown that different types/subtypes of MCI can progress into different types of dementia at varying rates. The models we

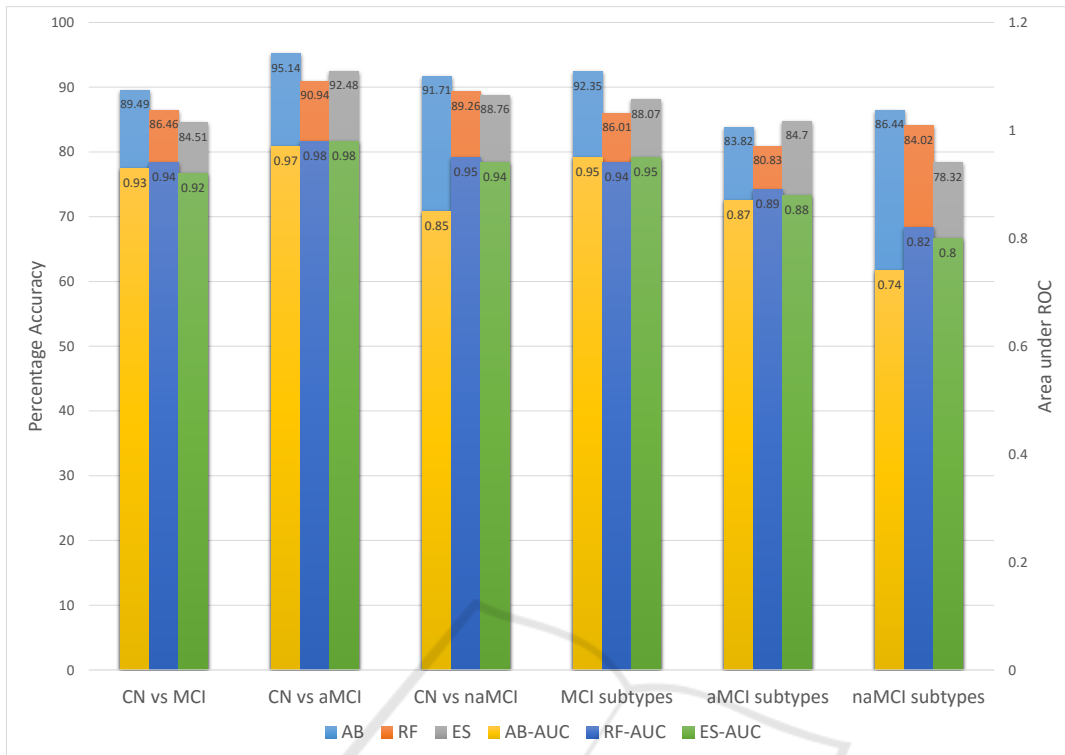


Figure 1: Best accuracies and AUC for each model grouped together for each one vs one class.

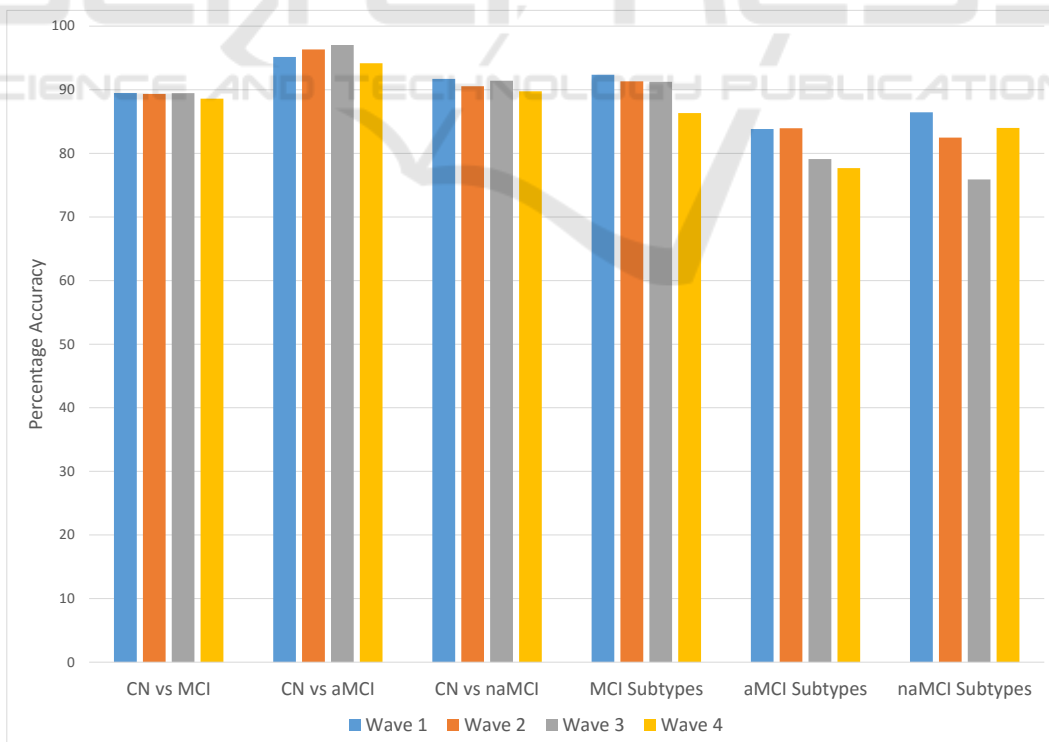


Figure 2: Best accuracies for each wave grouped together for each one vs one class. The lowest AUC is 0.77 while the mean AUC is around 0.86.

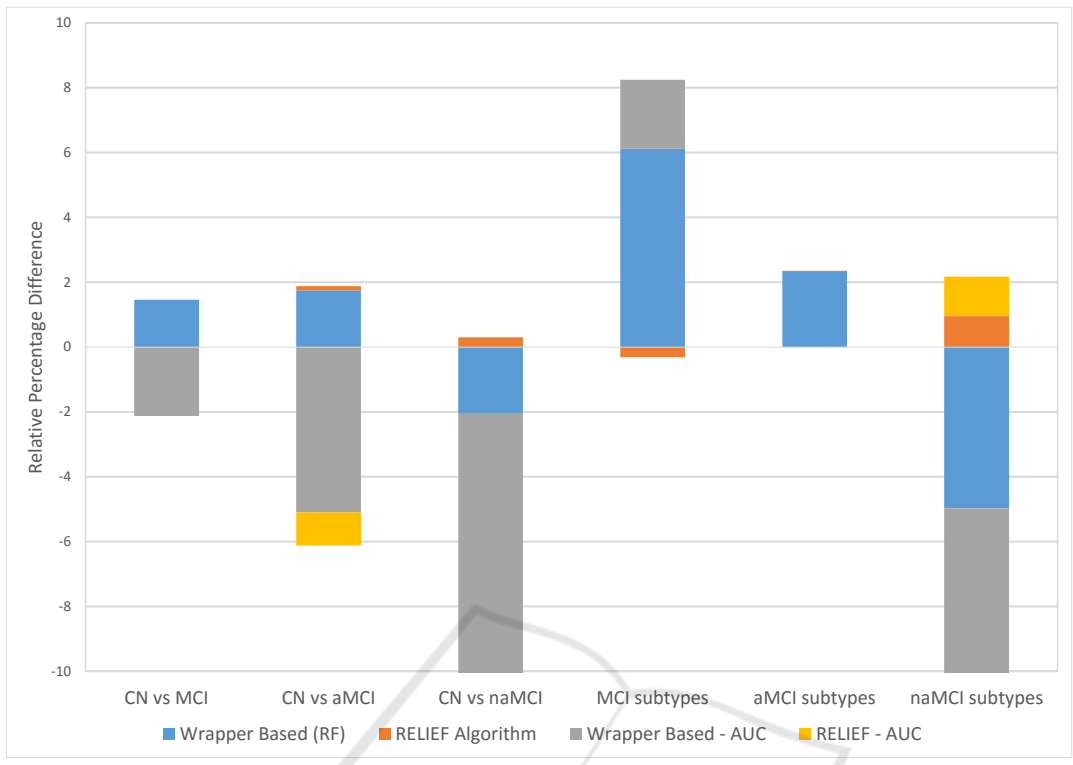


Figure 3: The percentage differences after feature selection for models trained using random forest. The minimum value of the plot is cut-off at -10 for clarity although two data points lie outside the range. Both data points correspond to AUC values of wrapper based feature selection; -18.94% for CN vs naMCI and -39% for naMCI subtypes.

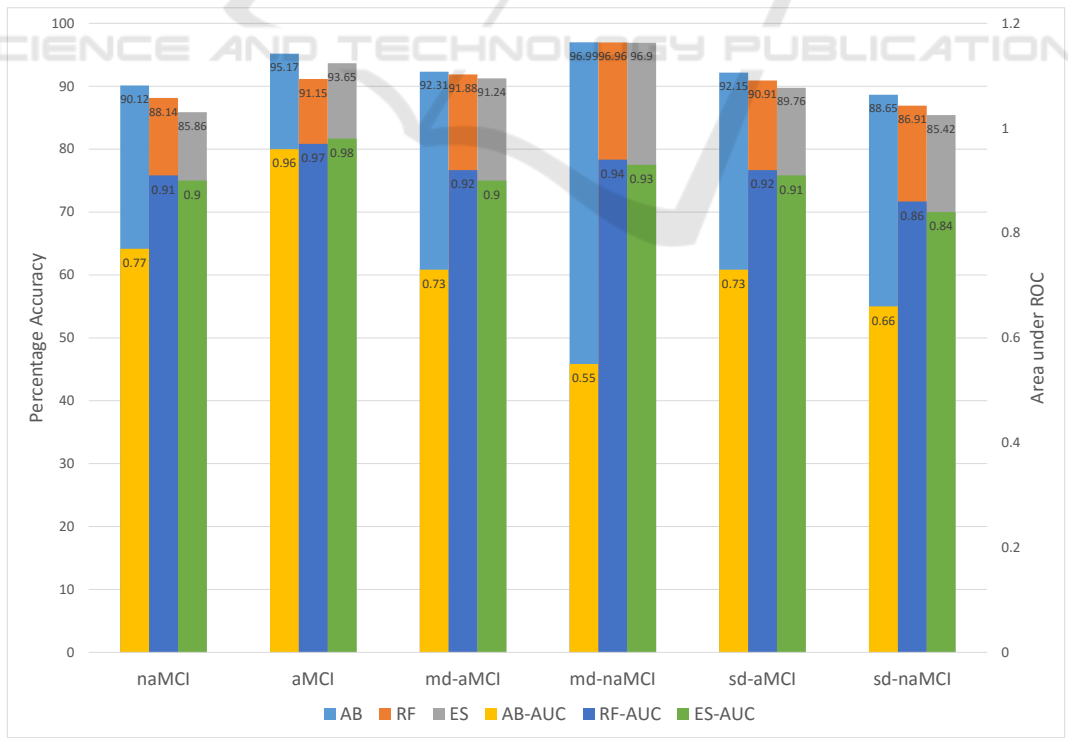


Figure 4: Best accuracies and AUC for each model grouped together for each one vs all class.

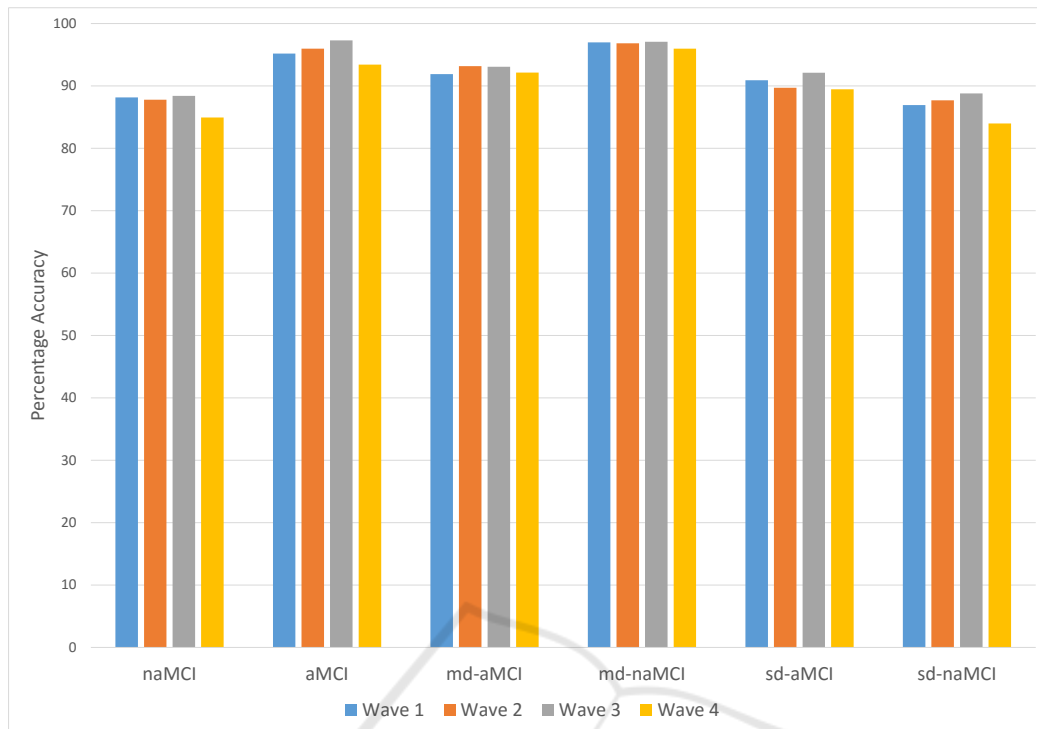


Figure 5: Best accuracies for each wave grouped together for each one vs all class. The lowest AUC is 0.85 while the mean AUC is around 0.92.

have trained using neuropsychological measures have excellent classification performance with a high level of accuracy without compromising the generalizing capabilities of the model, as seen from the high values of AUC.

Many published studies concentrate on differentiating between MCI and its subtypes (Raamana et al., 2014; Haller et al., 2013). However, only one of them used purely neuropsychological measures to train their models (albeit for a related but different classification). Most studies use image based features such as morphological MR images or diffusion tensor images. The study that used neuropsychological measures trained their classifier to differentiate between MCI and AD rather than CN/MCI and its subtypes (Lemos et al., 2012). For this reason, we cannot draw a direct comparison from the available literature. However, we have presented comparisons with two of the closest studies that we could find that used neuropsychological features. In addition, we also draw a comparison to a similar classification task that used the same dataset. Clearly our results are of the same calibre or often times better than the aforementioned studies. Perhaps what validates our results the most is that we are using one of the largest datasets reported in the literature, which improves the general-

ization capabilities of our trained models. The sample size coupled with repeated cross validation ensures minimization of overfitting as well. In addition, the best performing classifiers in the experiment were obtained using AdaBoost, Ensemble Selection and random forest, which are inherently robust against overfitting. As our experimental setup is optimized to avoid overfitting as much as possible while improving the accuracy by fine-tuning the parameters, we believe our results demonstrate superior performance.

It should be noted that there is a degree of circularity in using neuropsychological measures to differentiate between MCI subtypes as the same neuropsychological measures were used to come up with labels for each sample. However, the labeling process can be considered as a weak classifier in itself as it tends to follow a set of rules much like a rule based classifier that was manually designed. However, when the experts disagree with the labels assigned by the rules, the case labels are changed actively. Therefore, the labeling process may be considered as a basic set of rules with a dynamic set of exceptions as labeling progresses. We believe this unique labeling process partially explains the reason for boosting and ensemble methods to have performed better in the experiments as boosting/ensemble methods can be used to improve

the performance of a weak learner and expand its coverage by including more features. We also believe this opens up a direction for future work as NM and MRI based features can be considered as two independent datasets which leads to the paradigm of multi-view learning. We intend to explore this in the future.

Although the results of feature subset selection are not entirely successful, it may still prove useful. For large datasets, the best improvement in performance is demonstrated with random forest wrapper based feature selection. Performance is worse for CN vs naMCI and naMCI subtypes. The reason can be explained when we look at the sample sizes. In the naMCI subtype classifier, there are 122 instances for md-naMCI and 26 instances for sd-naMCI. With a wrapper based feature selection method, the training set becomes even smaller, which explains the relative decrease in AUC of around 40% from 0.82 to 0.5.

It is interesting to observe that, while most related literature report good performance with SVM, it was one of the worst performing classifiers in our experiments. Although it has been considered as the default classifier in recent times, our experiments suggest otherwise for the selected domain and problem. It is worthwhile to understand the structure of the dataset we are dealing with before choosing a classifier and we believe the nature of the data we are dealing with explains why tree structures perform better than other methods.

In future, we intend to utilize neuropsychological measures to predict progression from CN to MCI as well as MCI to AD. This may prove invaluable in identifying individuals at risk of MCI and AD so that they can be closely monitored and treated better. We also intend to combine neuropsychological measures with image based features derived from modalities such as morphological MRI and diffusion tensor images, in an attempt to improve the reported performance in literature. We believe the key to performance enhancement lies in understanding the structure of the dataset and designing customized classifiers best fitted for the dataset in question.

In conclusion, we strongly believe that it is a worthwhile effort to automate diagnosis of MCI and its subtypes. Generally MCI is diagnosed in the older population, and for a considerable number of patients, MRI scans may be contraindicated because they have pacemakers or other implants, have muscular-skeletal issues or are claustrophobic. Furthermore there is the high cost of MRI scans. Reliable diagnosis of MCI using neuropsychological measures would therefore have considerable advantage. To that extent, we believe the models we have trained and validated can be a great starting point.

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