Measuring the Latency of an Augmented Reality System for Robot-assisted Minimally Invasive Surgery

Martin Kibsgaard and Martin Kraus

Department of Achitecture, Design and Media Technology, Aalborg University, Aalborg, Denmark

Keywords: Augmented Reality, Latency, Teleoperation, Telepresence, Medical Training, Robot-assisted Surgery.

Abstract: Minimal latency is important for augmented reality systems and teleoperation interfaces as even small increases in latency can affect user performance. Previously, we have developed an augmented reality system that can overlay stereoscopic video streams with computer graphics in order to improve visual communication in training for robot-assisted minimally invasive surgery with da Vinci surgical systems. To make sure that our augmented reality system provides the best possible user experience, we investigated the video latency of the da Vinci surgical system and how the components of our system affect the overall latency. To measure the photon-to-photon latency, we used a microcontroller to determine the time between the activation of a light-emitting diode in front of the endoscopic camera and the corresponding increase in intensity of the surgeon's display as measured by a phototransistor. The latency of the da Vinci S surgical system was on average 62 ms. None of the components of our overlay system (separately or combined) significantly affected the latency. However, the latency of the assistant's monitor increased by 14 ms. Passing the video streams through CPU or GPU memory increased the latency to 147 ms and 256 ms, respectively.

1 INTRODUCTION

During training for robot-assisted minimally invasive surgery, visual communication is limited as the immersive interfaces of most surgical robots block the line of sight between instructors and trainees. To better support visual communication during training on the da Vinci surgical systems, we have developed a system that overlays the stereoscopic video streams with computer graphics. We describe the system in detail in (Kibsgaard and Kraus, 1999) and a specific application of the system in (Kibsgaard and Kraus, 2016). The core of the system is a computer with two video capture cards that can overlay the video streams with low latency.

The system intercepts the main video streams between the camera control units and the surgeon's console that is used to control the robot. Even though the video capture cards can overlay the video streams in less than 1 millisecond, we know from previous experience (Matu et al., 2014) that introducing additional latency can affect the overall latency significantly more than just the time it takes to overlay the video streams. Unfortunately, increasing overall latency of teleoperation in augmented reality or virtual reality systems reduces user performance and increases error rates (Azuma et al., 2001; Ellis et al., 1997; Ware and Balakrishnan, 1994).

In this paper, we investigate the video latency of the da Vinci surgical system and how our system and its components affect the overall latency. In Section 2, we present the current setup of our system and how others have measured latency of augmented reality systems. The approach we use to measure latency and a description of different overlay setups and components is described in Section 3. The measured latencies of the different setups are presented and discussed in Section 4.

2 PREVIOUS WORK

Most previous works on augmenting the video streams of the da Vinci surgical systems introduce significant additional latency on the video signals. Many approaches (Ali et al., 2008; Su et al., 2009; Matu et al., 2014; Jarc et al., 2016) transfer image data from the video streams to a CPU and in some cases also to a graphics card, which in both cases results in more than 100 ms additional latency of the video signals. Azuma et al. claimed that delays as small as 10 ms can have a negative effect on user performance for

Kibsgaard M. and Kraus M.

DOI: 10.5220/0006274203210326

In Proceedings of the 12th International Joint Conference on Computer Vision, Imaging and Computer Graphics Theory and Applications (VISIGRAPP 2017), pages 321-326 ISBN: 978-989-758-224-0

Copyright © 2017 by SCITEPRESS - Science and Technology Publications, Lda. All rights reserved

Measuring the Latency of an Augmented Reality System for Robot-assisted Minimally Invasive Surgery.



Figure 1: Overview of the setup we use to overlay the video streams of the da Vinci S surgery system with computer graphics including failsafes and a 3D TV. Grey: standard da Vinci S components. Blue: overlay system (video capture cards in a computer). Green: Mini-converters used as loss-of-signal switches. Yellow: 3D HDMI conversion and 3D TV.

some tasks (Azuma et al., 2001), thus an additional 100 ms latency is unwanted. The approaches that can overlay the video streams with low latency only work with the SD-SDI format of the first generation robot (Figl et al., 2010) or employed now obsolete and discontinued hardware (Hattori et al., 2003).

Our system (Kibsgaard and Kraus, 1999) uses two 2nd generation DeckLink HD Extreme video capture cards to overlay the HD video streams of the da Vinci S surgical system with computer graphics: one video capture card for the left channel and one for the right channel. To generate the computer graphics, we have integrated the DeckLink API with the popular Unity game engine. The system generates stereo graphics using a virtual camera setup that is similar to the endoscope of the surgery robot and outputs it through the DeckLink cards using internal keying (overlaying). The manufacturer of the video capture cards, Blackmagic Design, claims that the internal keying introduces less than 1 millisecond of additional latency on the video stream passing through the video capture cards The hardware setup and connections for the overlay system are illustrated in detail in Figure 1.

The output of each of the two video capture cards is connected to separate SDI-to-HDMI converters along with the redundant output of each camera control unit of the surgery robot, which are connected to the converters' alternate input. In this configuration, the converters function as loss-of-signal switchers that revert the video streams to the original video signal in case the overlay system malfunctions and/or is shut down.

The standard da Vinci S surgical system provides monoscopic monitors for assistants and instructors. To provide them with a stereoscopic view of the surgery field and the computer graphics, our system also includes a Matrox MC-100 Dual-SDI-to-3D-HDMI converter which is connected to a 3D TV with passive stereo glasses. The MC-100 is connected between the loss-of-signal switchers and the surgeon's console to make sure that the 3D TV always shows the same images as the console. The drawback of this placement is that the video signals rely on an additional component even when the rest of the overlay system is off.

Previous works that measure latency of augmented reality systems with video see-through displays distinguish between two categories of latency: photon-to-photon latency and motion-to-photon latency. The first is in some cases also called visual latency and relates to the time it takes from a photon entering a camera until a corresponding photon is emitted and visible on a display. In our case, that is the latency between light entering the stereoendoscopic camera until it is displayed on the surgeon console's displays. Motion-to-photon latency is sometimes called *input latency* and is the time from the user providing an input to a corresponding change that is visible on a display. As our overlay system only affects the video streams, measuring the photon-tophoton latency is sufficient for measuring how much the motion-to-photon latency is affected by our system.

To measure photon-to-photon latency, Jacobs et al. placed a light emitting diode (LED) in front of a camera and powered the LED using a low frequency signal generator (Jacobs et al., 1997). They placed a photoelectric sensor on the display and connected it and the signal generator to an oscilloscope. The photon-to-photon latency could then be determined by the oscilloscope as the time offset between the two signals. Because of the discrete nature of video, the measured latency is dependent on when the LED is triggered in relation to the shutter of the camera. To get a representative sample, the measurements have to be repeated many times. This setup is most useful if only a few setups have to be measured.

To automatically record the measurements, Blissing and Bruzelius replaced the signal generator and oscilloscope with a computer (Blissing and Bruzelius, 2015). This makes it possible for the computer to quickly measure multiple times and correlate the measurements with events and performance of the host computer. They provide no specifics on the hardware and software that was used to obtain the measurements. Bachhuber and Steinbach implemented similar test equipment using an Arduino Uno microcontroller to control the LED and measure the change in light intensity of the display (Bachhuber and Steinbach, 2015). The microcontroller samples the lightto-voltage sensor at 2 kHz achieving a resolution of 0.5 ms.

Sielhorst et al. proposed a setup that can measure the absolute latency more precisely with fewer measurements (Sielhorst et al., 2007). It does so by recording the display of the augmented reality system with the camera of the same system. It is then able to measure the time it takes from the time when the overlay system outputs an image to the time when the same image is captured by the camera and it arrives in system memory. However, as some of the setups that we are interested in do not pass the image data through system.

3 MEASURING LATENCY

3.1 Test Equipment

To measure photon-to-photon latency of our overlay system, we have developed test equipment that is similar to previously proposed setups (Bachhuber and Steinbach, 2015; Blissing and Bruzelius, 2015) using basic electronic components and a microprocessor. A light emitting diode (LED) controlled by a microcontroller is placed in front of the stereoscopic camera and a high-speed light-to-voltage sensor is placed in front of the display in the surgeon's console (Figure 2). To determine the photon-to-photon latency, the microcontroller switches on the LED and measures the time it takes to detect the corresponding rise in light intensity of the display.

A schematic of the circuit that is connected to the microcontroller can be seen in Figure 3. The LED we chose is a high brightness white LED to ensure a significant change in intensity of the display. The lightto-voltage sensor is a visible-light phototransistor in series with a resistor. The varying voltage from the sensor is connected to the built-in voltage comparator



Figure 2: Test setup. Left: LED in front of endoscopic camera (without lens). Right: Light to voltage sensor in front of displays in the surgeon's console. Both were covered during measurements to block light from the environment.

of the ATmega328P microcontroller on an Arduino Uno. This makes it possible for the microcontroller to immediately trigger and stop timing when the sensed voltage rises past a set threshold. The benefit of this approach is that it provides a higher resolution (4 μ s vs. 100 μ s) compared to sampling at a fixed frequency in previous works (Bachhuber and Steinbach, 2015; Blissing and Bruzelius, 2015). However, this prevents us from using an automatic threshold adjustment and filtering (Bachhuber and Steinbach, 2015). The reference voltage for the comparator (threshold) is instead set by an external potentiometer that has to be adjusted to match the monitor's intensity range.

To automate the measurements further, we implemented a simple application that communicates with the microcontroller via USB (UART). The application can start tests and save the results to a file with a user-specified number of measurements and file name. To avoid aliasing artefacts, a random delay is introduced between each measurement. The delay has to be larger than the highest measured latency to avoid triggering on the previous measurement's intensity change. Source code is available at https://github.com/Kibsgaard/latency-measurement.

To avoid that other light sources in the environment affect the measurements, we covered the camera and display with opaque sheets of fabric. This also makes it possible to set the threshold of the comparator lower, which makes the system react faster to rises in light intensity.



Figure 3: Schematic of the test equipment. The labels are based on Arduino Uno pin mapping. "A0" and "A1" are used during calibration.

3.2 Overlay Setups

To measure our system's effect on the photon-tophoton latency we used the test equipment with the da Vinci S surgical system where our system is installed and used during training at Aalborg University Hospital. The installed overlay system uses two Deck-Link HD Extreme 2 video capture cards, two SDIto-HDMI converters and one Matrox MC-100 SDIto-3D-HDMI converter. Note that the SDI-to-HDMI converters are only used as loss-of-signal switchers and the HDMI signal is not used. The MC-100 outputs both a 3D-HDMI signal for the 3D TV and passthrough SDI signals that are connected to the surgical system. We measured the latency of multiple combinations of the components to investigate their individual and combined latency as well as to see if any combination of the components has an effect on the synchronization of the signals.

Furthermore, we tested the system with different DeckLink video capture cards to investigate claims of slower internal keying (1-2 frames) on some of the newer generation cards (Jefferson, 2015). In one setup, we exchanged the DeckLink HD Extreme 2 cards with a DeckLink 4K Extreme card and in another setup with a DeckLink Quad 2 card. Furthermore, we measured the photon-to-photon latency of the assistant's monitor both with and without the attached overlay system. The latency of the installed 3D TV was also measured to compare it to the standard monitor that is available to the assistants.

With the current setup, the image data from the video signals is never transferred to the system memory of the computer that overlays the video streams with computer graphics. Instead, the computer sends the computer graphics to the video capture card, which then overlays the incoming video signal a few lines at a time and immediately outputs them. Thus, it is not possible for the system to do any form of image processing on the incoming data (apart from the alpha blending that is used for overlaying). By using a DeckLink Quad it is possible to transfer the image data to system memory, modify it and output it again; although with a significant latency increase as it has to wait for a complete frame (33.3 ms) and do at least two memory transfers.

The newer DeckLink Quad 2 is capable of keying HD video signals, which makes it possible to input the image data and process it while simultaneously overlaying the input signals with computer graphics. Note that the image data still arrives later in system memory compared to the signal being overlaid, which results in delayed graphics in cases where the graphics rely on information from the processed image data.



Figure 4: Photon-to-photon latency (in ms) of the da Vinci S surgical system with various configurations of our system. ("L" stands for loss-of-signal switchers; "M" for the MC-100 SDI-to-3D-HDMI converter.) The blue " \times " marks the average latency.

In addition, we also measure the latency introduced by transferring the image data to a graphics card's memory, modifying it and copying it back. This was done using sample code from the Deck-Link SDK. The overlay system has a NVIDIA Quadro 4000 graphics card, which makes it possible to utilize GPUDirect. This feature removes one memory copy operation by giving the video capture card and graphics card access to the same system memory. However, the image data still has to be copied from the video capture card to system memory and then to the graphics card's memory (and back again).

The last setup we measured was using a video switcher with built-in keying functionality instead of keying using the DeckLink cards. We tested this with the Blackmagic Design ATEM Television Studio that supports downstream, chroma and luma keying.

4 **RESULTS**

All measurements were performed on a da Vinci S surgical system, which uses a video signal with a 1080i video format and a refresh rate of 59.94 fields per second. (One frame of an interlaced video format consists of two fields.) We measured the inherent photon-to-photon latency of the standard da Vinci S surgical system to be 62.4 ms (SD = 4.7 ms, N = 1000) with a minimum measurement of 54.0 ms and maximum of 70.7 ms. As shown in Figure 4, there were no noticeable differences in measured latency between the surgery system without and with the overlay system that we presented previously (Kibsgaard and Kraus, 1999). This includes different combinations of components and measurements with the newer generation DeckLink video capture cards, DeckLink 4K Extreme and DeckLink Quad 2, which

were claimed to introduce higher latency (Jefferson, 2015).

The measurements are evenly spread and stayed within the duration of one field (16.7 ms). This indicates that the displays of the surgeon's console are well synchronized with the camera control units and none of the setups displayed in Figure 4 disrupted this synchronization.

The measurements of the assistant's monitor (telestrator) are more spread and here the overlay system has a noticeable effect on the photon-to-photon latency (Figure 5). The latency of the telestrator is on average 110.7 ms (SD = 8.0 ms, N = 1000) without the overlay system and 125.1 ms (SD = 7.6 ms, N = 1000) with the attached overlay system resulting in 14.3 ms increased latency.

As shown in Figure 6, passing the image data through the overlay system's memory increases the photon-to-photon latency from the endoscopic camera to the surgeon's console significantly. By transferring the image data to system memory, modifying a few pixels using the CPU and immediately outputting it through the DeckLink cards, the photon-to-photon latency is increased by 84 ms to an average of 145.6 ms (SD = 4.9 ms, N = 999). One extreme outlier (50 ms), which was lower than the inherent latency of the system, was removed from the measurements. It is possible that the light sensor was not completely covered and it got prematurely triggered by changing light in the environment.

If the data is also transferred to the graphics card, modified and transferred back, the latency is increased by 177 ms to an average of 237.7 ms (*SD* = 7.8 ms, N = 100). Utilizing NVIDIA's GPUDirect feature does not reduce this latency significantly (0.9 ms lower). However, it does reduce the amount of work the CPU has to do and utilizes asynchronous readback from the graphics card. As previously mentioned, these tests were done using the pass-through examples from the DeckLink SDK. As shown in Figure 6, the DirectX example had some very high latency measurements and dropped several frames, which caused the displays to blink. The cause of this is unknown.

Using the keying functionality of the ATEM Television video switcher adds close to one field of la-



Figure 5: Photon-to-photon latency (in ms) from the endoscopic camera to the assistant's display. The blue " \times " marks the average latency.

Quad 2 CPU	H X H					
Quad 2 GPU			H X	H		
Quad 2 DirectX GPUDirect				<		
Quad 2 OpenGL GPUDirect		⊢ <u></u> ₩→				
	130	180	230	280	330	380



tency when chroma keying (79.5 ms (SD = 5.2 ms, N = 100)) and two fields (one frame) of latency when using luma keying (96.2 ms (SD = 4.8 ms, N = 100)) or downstream keying (96.1 ms (SD = 5.0 ms, N = 100)). Thus, it is not able to replace the functionality of the DeckLink video capture cards in our overlay system.

Additionally, we measured the photon-to-photon latency from the endoscopic camera to the 3D TV (including loss-of-signal switchers and SDI-to-3D-HDMI converter) to be 181.9 ms (SD = 5.0 ms, N = 1000), which is 71.2 ms higher than the telestrator (110.7 ms).

5 CONCLUSIONS

We have measured the photon-to-photon latency of the da Vinci S surgical system with and without a previously presented system that can overlay the video streams with computer graphics. The latency of the surgery system from the endoscopic camera to the surgeon's display was measured to be 62 ms, and the overlay system has no significant effect on that latency. However, the overlay system does increase the photon-to-photon latency from the endoscopic camera to the assistant's display by 14.3 ms on average.

The overlay system consists of two video capture cards in a computer, two loss-of-signal switchers and an SDI-to-3D-HDMI converter. The newer generation video capture card DeckLink Quad 2 can replace the two cards in the previously proposed system as it has similar latency, is more accessible, offers more functionality, and is more compact.

With the current system, the image data from the video streams is not transferred to system memory to avoid excessive additional latency. Passing the data through system memory increases the photon-to-photon latency to 147 ms and further to 256 ms when transferred to the graphics card and back.

6 FUTURE WORK

Passing the image data from the video streams through system memory with our current setup is too slow for real-time interaction, especially in cases where the graphics card needs to have access to the data. AMD's DirectGMA might be faster than NVIDIA's GPUDirect, as it enables the video capture cards to access graphics card memory directly without an intermediate transfer through system memory.

An alternative approach is to use a DeckLink Quad 2 to overlay the video streams while simultaneously using two other channels of the Quad 2 to capture and process the image data. Future work should investigate how a system where the overlaid graphics are delayed affect user acceptance and how to design around that problem (e.g. by extrapolating motion).

Future work could also involve measuring the latency of video capture cards by other manufactures, the motion-to-photon latency of the surgical system and further investigate the increased latency of the assistant's display when our system is active.

ACKNOWLEDGEMENTS

We thank the staff of the Department of Urology at Aalborg University Hospital and Minimal Invasiv Udviklings Center for sharing their expertise with us and providing access to their training system.

REFERENCES

- Ali, M. R., Loggins, J. P., Fuller, W. D., Miller, B. E., Hasser, C. J., Yellowlees, P., Vidovszky, T. J., Rasmussen, J. J., and Pierce, J. (2008). 3-d telestration: a teaching tool for robotic surgery. *Journal of Laparoendoscopic & Advanced Surgical Techniques. Vol. 18, Issue 1*, pages 107–112.
- Azuma, R., Baillot, Y., Behringer, R., Feiner, S., Julier, S., and MacIntyre, B. (2001). Recent advances in augmented reality. *IEEE Computer Graphics and Applications*, 21(6):34–47.
- Bachhuber, C. and Steinbach, E. (2015). A System for Precise End-to-End Delay Measurements in Video Communication. *IEEE International Conference on Image Processing (ICIP 2016).*
- Blissing, B. and Bruzelius, F. (2015). A technical platform using augmented reality for active safety testing. *Road Safety & Simulation International Conference Proceedings*, (October 2015):793–803.
- Ellis, S., Breant, F., Manges, B., Jacoby, R., and Adelstein, B. (1997). Factors influencing operator interaction with virtual objects viewed via head-mounted

see-through displays: viewing conditions and rendering latency. *Proceedings of IEEE 1997 Annual International Symposium on Virtual Reality*, pages 138– 145.

- Figl, M., Rueckert, D., Hawkes, D., Casula, R., Hu, M., Pedro, O., Zhang, D. P., Penney, G., Bello, F., and Edwards, P. (2010). Image guidance for robotic minimally invasive coronary artery bypass. *Computerized Medical Imaging and Graphics: The Official Journal of the Computerized Medical Imaging Society*, 34(1):61–68.
- Hattori, A., Suzuki, N., Hashizume, M., Akahoshi, T., Konishi, K., Yamaguchi, S., Shimada, M., and Hayashibe, M. (2003). A robotic surgery system (da vinci) with image guided function–system architecture and cholecystectomy application. *Studies in Health Technology* and Informatics, 94:110–116.
- Jacobs, M. C., Livingston, M. A., and State, A. (1997). Managing latency in complex augmented reality systems. In *Proceedings of the 1997 symposium on Interactive 3D graphics - SI3D '97*, pages 49–ff., New York, New York, USA. ACM Press.
- Jarc, A. M., Shah, S. H., Adebar, T., Hwang, E., Aron, M., Gill, I. S., and Hung, A. J. (2016). Beyond 2D telestration: an evaluation of novel proctoring tools for robot-assisted minimally invasive surgery. *Journal of Robotic Surgery*, 10(2):103–109.
- Jefferson, M. (2015). Blackmagic Forum View topic Internal keyer and channels on Decklink Quad 2.
- Kibsgaard, M. and Kraus, M. (1999). Real-time augmented reality for robotic-assisted surgery. In *The 3rd AAU Workshop on Robotics: Proceedings*, pages 19–23. Aalborg Universitetsforlag.
- Kibsgaard, M. and Kraus, M. (2016). Pointing with a oneeyed cursor for supervised training in minimally invasive robotic surgery. In Lecture Notes in Computer Science (including subseries Lecture Notes in Artificial Intelligence and Lecture Notes in Bioinformatics), volume 9515, pages 12–21. Springer, Cham.
- Matu, F. O., Thøgersen, M., Galsgaard, B., Jensen, M. M., and Kraus, M. (2014). Stereoscopic augmented reality system for supervised training on minimal invasive surgery robots. In *Proceedings of the 2014 Virtual Reality International Conference on - VRIC '14*, pages 1–4, New York, New York, USA. ACM Press.
- Sielhorst, T., Sa, W., Khamene, A., Sauer, F., and Navab, N. (2007). Measurement of absolute latency for video see through augmented reality. In 2007 6th IEEE and ACM International Symposium on Mixed and Augmented Reality, ISMAR, pages 1–4. IEEE.
- Su, L. M., Vagvolgyi, B. P., Agarwal, R., Reiley, C. E., Taylor, R. H., and Hager, G. D. (2009). Augmented Reality During Robot-assisted Laparoscopic Partial Nephrectomy: Toward Real-Time 3D-CT to Stereoscopic Video Registration. Urology, 73(4):896–900.
- Ware, C. and Balakrishnan, R. (1994). Reaching for objects in VR displays: lag and frame rate. ACM Transactions on Computer-Human Interaction, 1(4):331–356.