Multilabel Classification of Otoscopy Images in Deep Learning for Detailed Assessment of Eardrum Condition

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- Keywords: Otoscopy Imaging, Multi-Label, Convolutional Neural Network.
- Abstract: This study presents a ResNet50-based CNN framework for multi-label classification of eardrum images, focusing on a detailed diagnosis of otologic disorders. Unlike prior studies centered on common pathologies, our approach explores less common eardrum conditions using a dataset of 4836 images annotated by two audiologists. The model effectively identifies various pathologies and conditions that can coexist in clinical practice, with a Jaccard score of 0.84, indicating a high level of agreement with the annotations made by an expert. This score notably exceeds the interoperator agreement (0.69) between the two audiologists. This demonstrates the model's accuracy but also its potential as a reliable tool for clinical diagnosis.

1 INTRODUCTION

Otoscopy has significantly advanced with Deep Neural Networks (DNNs), especially Convolutional Neural Networks (CNNs), revolutionizing medical image classification (LeCun et al., 2015) and sometimes outperforming human experts (Gulshan et al., 2016). The adoption of the CNN multilabel classification in otoscopy, which enables the simultaneous identification of multiple ear pathologies, aligns closely with realworld clinical complexities, improving diagnostic relevance.

Recent studies using otoscopic images have predominantly applied binary (Habib et al., 2023b; Habib et al., 2023a) or multiclass (Zeng et al., 2021; Cha et al., 2019; Wu et al., 2020) classification approaches with very good results: 92.1% with InceptionResnet-v2 and 3 classes (Cha et al., 2019), 95.59% with DenseNet and 8 classes (Zeng et al., 2021), 97.47 with MobileNet and 3 classes (Wu et al., 2020), 84.4% with a custom CNN and 3 classes (Livingstone et al., 2019), 91% with DenseNet and 1 class (Habib et al., 2023a), often limiting the scope to a few common pathologies (Chen et al., 2022; Zeng et al., 2021; Viscaino et al., 2020; Wu et al., 2020; Livingstone et al., 2019). These approaches, while useful, falls short in clinical settings where a broad spectrum of ear conditions, including rare diseases, may be present (Cha et al., 2019). In fact the number of pathologies examined in these studies has been typically low, restricting the ability to provide comprehensive diagnostic insights.

In contrast, our research focuses on advanced otoscopy image analysis through multi-label classification enabling several tympanic conditions to be identified simultaneously, with a novel approach: we tested several Convolutional Neural Network (CNN) architectures and finally tailored a ResNet model for our purpose. Our study uniquely encompasses an extensive array of 18 ear pathologies and conditions, including those seldom seen in clinical settings. This broad spectrum approach enables us to provide a nearcomplete description of various eardrum states.

Our objective is to narrow the gap between highperforming artificial intelligence models and their real-world applicability in diverse medical scenarios. This paper outlines our methodology and showcases the results from our cutting-edge approach.

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2 MATERIALS AND METHODS

2.1 Description of the Otoscopy Dataset

We used a dataset from the "Auditis Clinic" in Reims, France, which consists of 4836 otoscopy images, each of size 720px by 720px. These eardrum images were annoted by two audiologists, henceforth denoted from here on by **E1** and **E2**, in a multi-label context, with up to 3 labels per image, to ensure an accurate description of the condition of every imaged eardrum.

Figure 1 illustrates the variability in labeling tympanic membranes by two experts. For instance, image **c** received conflicting labels of *Normal* (E2) and *Atelectatic Otitis* (E1), while image **f** was differently labeled as *Cholesteatoma* and *SOM*. This highlights the challenges in consistent eardrum labeling, as an eardrum can appear normal but still present a pathology. Consensus was, for the *Cholesteatoma* label, reached only in image **h**, with disagreement on images **g** and **i**, marked as *Normal* and *Tympanosclerosis*. These inconsistencies emphasize the need for standardized, automated eardrum image analysis.

The dataset (Table 1) shows a skewed label distribution due to subject pre-selection. Most ears have

been previously assessed by otolaryngologists, resulting in an over-representation of the *Normal* label. This contrasts with the 17 other labels indicating various ear conditions. Such skewness is crucial to consider in machine learning model training to avoid bias towards the *Normal* condition. Additionally, some labels denote conditions that are inherently challenging to detect, leading to diagnostic variability, as illustrated above.

Figure 2 presents confusion matrices for every label, highlighting the agreement level between the two experts in our multi-label classification task. These matrices exclude True Negatives and are normalized by L, which represents the number of images labelled with the pathology by at least one expert. The presented confusion matrices illustrate the highly variable degrees of agreement between experts, depending on the pathology. For example, Ventilation Tube (Jaccard Score: J = 1.00, see Eq. 5) and Partial Obstruction (J = 0.87) exhibit high concordance, whereas Serous Otitis Media (J = 0.03) and Cholesteatoma (J = 0.04) show low agreement. This indicates differing opinions or diagnostic ambiguity among experts. Note that on this scale, a Jaccard Score is considered high when it reaches 0.6 or above,

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Figure 2: Confusion matrices presenting Labels (i.e. ear conditions) repartition over experts, and variability in eardrum pathology labelization.

and very good to excellent when it falls between 0.8 and 1. E1 generally uses a broader array of labels per image (average: 1.50 ± 0.63), suggesting a more inclusive approach. In contrast, E2 averages fewer labels (1.25 ± 0.48), indicating a focus on prominent features. This variance in labeling strategies is significant, with E1 identifying 2710 problematic images compared to E2's 2335.

2.2 Performance Evaluation Metrics

In evaluating our multilabel otoscopy labeling system, we focus on key metrics: **precision** (p), **recall** (r), and **F1 score** (Olson and Delen, 2008). Precision, indicating the accuracy of positive predictions, is crucial in medical contexts as it minimizes false positives. Recall, reflecting the ability to identify all positive cases, is vital to reduce missed diagnoses. F1 score provides a balanced view of the overall performance.

Label	E1	E2
Earwax Plug	228	181
Normal	3795	3404
Tympanosclerosis	1088	420
Osteomas	173	174
Atelectatic Otitis	114	82
Otorrhea	46	39
Ventilation Tube	32	32
External Otitis	64	28
Mastoid Cavity	35	39
Partial Obstruction	1236	1165
Unlabelable	18	205
Cholesteatoma	15	150
Acute Middle Otitis	26	15
Pseudotympanum	209	60
Serous Otitis Media	71	3
Stenosis	29	9
Tympanic Perforation	100	63
Foreign Body	7	9

Table 1: Summary of ear conditions with the number of cases labeled by two experts (E1 and E2).

In multi-label classification, particularly with imbalanced datasets, the **samples average F1 score** is often preferable as it calculates the F1 score for each individual sample and then averages these scores; each sample is so treated equally, regardless of its label combination, ensuring that the model's ability to predict all possible label combinations is evaluated and not just the more frequently occurring labels or classes. The formula for the **samples average F1 score**, incorporating precision and recall calculations with label-specific vector notation, is given by:

$$F1 = \frac{1}{N} \sum_{i=1}^{N} F1_i$$
 (1)

with

$$p_i = \frac{\sum_k \operatorname{TP}_i(k)}{\sum_k \operatorname{TP}_i(k) + \sum_k \operatorname{FP}_i(k)},$$
(2)

$$r_i = \frac{\sum_k \operatorname{TP}_i(k)}{\sum_k \operatorname{TP}_i(k) + \sum_k \operatorname{FN}_i(k)},$$
(3)

$$F1_i = \frac{2 \times p_i \times r_i}{p_i + r_i} \tag{4}$$

where r_i and y_i are vectors of K elements (K=18 ear conditions), representing respectively reference values and predicted values for image i; and $\text{TP}_i(k) = 1$ if $\mathbf{y}_i(k) = \mathbf{r}_i(k) = 1$ (true positive for label k in image i), $\text{FP}_i(k) = 1$ if $\mathbf{y}_i(k) = 1$ and $\mathbf{r}_i(k) = 0$ (false positive), $\text{FN}_i(k) = 1$ if $\mathbf{y}_i(k) = 0$ and $\mathbf{r}_i(k) = 1$ (false negative), and N the number of images.

The **Jaccard Score** is key in non-exclusive class models, such as in medical multi-label classification where multiple diagnoses may coexist. It measures the similarity between predicted and true label sets. The **samples average Jaccard Score** is calculated as:

$$J = \frac{1}{N} \sum_{i=1}^{N} \frac{\sum_{k} \operatorname{TP}_{i}(k)}{\sum_{k} \operatorname{TP}_{i}(k) + \sum_{k} \operatorname{FP}_{i}(k) + \sum_{k} \operatorname{FN}_{i}(k)}$$
(5)

which averages the Jaccard Scores for each image.

2.3 Experiments

Our exploration in neural network architectures for otoscopy image analysis involved evaluating a variety of models. This included a baseline Convolutional Neural Network (CNN) and several advanced models such as VGG16 (Simonyan and Zisserman, 2014), ResNet50 (He et al., 2016), DenseNet (Huang et al., 2017). All these models were pretrained on large datasets and subsequently adapted for otoscopy. This adaptation involved integrating a custom fully connected layer with a dropout layer to prevent overfitting on the training dataset. To address the challenges of label imbalance, we employed a weighted binary cross-entropy loss function (Zhou et al., 2021). This approach allows for the adjustment of weights inversely proportional to the frequency of the classes in the training data, thus giving higher importance to less frequent classes. Additionally, we utilized the Adam optimizer (Kingma and Ba, 2015), to facilitate more effective training of our neural network models. The training was conducted using TensorFlow and the computational work was performed on RTX 2080Ti GPU.

The training was a two-stage process, based on E1's labelisation: initially, the newly added layers were trained with the base model's weights fixed, followed by fine-tuning the entire network at a learning rate of 1e-5, thus balancing general and otoscopy-specific features.

For assessment, we used 5-fold cross-validation (Kohavi, 1995) with an 80-10-10 data partition for comprehensive evaluation.

Image consistency was maintained by standardizing resolutions to 128x128 pixels. Zoom/dezoom, contrast, and brightness variations were applied to enhance the dataset. Mirror augmentation (Shorten and Khoshgoftaar, 2019) further improved model generalization.

3 RESULTS

3.1 Overall Performance

Most models showed high Jaccard scores (Table2). ResNet50 excelled with a J = 0.84, outdoing the inter-annotator score of 0.79, indicating superior reliability. Six out of seven models surpassed this benchmark, as Table 2 shows. ResNet50, with a 0.01 standard deviation, displayed consistent performance across folds, highlighting its accuracy and generalization potential. DenseNet201 and VGG19 also performed well, scoring J = 0.82 and J = 0.81, respectively.

In refining our model for eardrum image classification, we employed threshold optimization on ResNet50, our top-performing architecture, to enhance prediction accuracy (Davis and Goadrich, 2006). This process involved iteratively testing different thresholds and assessing their impact on the F1 for each label on the validation set. By selecting label-specific thresholds that maximize the F1, we finely tuned the balance between false positives and negatives for each pathology. The subsequent classification report (Table 3) demonstrates final performance achieved with ResNet50.

On normal hearing, the F1 improved marginally from 0.94 to 0.95, indicating a slight enhancement in the model's accuracy for this prevalent condition. In the case of *Earwax Plug*, there was a notable increase in the F1 from 0.72 to 0.75, reflecting an improvement in both precision and recall for this condition. For *Partial Obstruction*, the F1 increased from 0.77 to 0.82.

However, for less represented classes, this process led to a decrease in performance. Notably, *Cholesteatoma* witnessed a reduction in F1, dropping from 1.00 to 0.67. This decrease suggests that while the model has become more adept at identifying more common conditions, it struggles with rarer. Final thresholds adjustments showed higher recall and lower precision.

3.2 Comparison with Human Inter-Observer Agreement

Key insights emerge from a comparison of Table 3 (ResNet50 metrics using E1's labels), Table 4 (comparison of expert annotations), and Table 5 (ResNet50 metrics using E2's labels for the most represented labels, i.e., labels that appear more than 200 times). These labels were chosen because they are the most commonly encountered by audioprosthetists, providing a sufficient number of images to effectively train

our CNN. It is important to note that the model used in Table 5 is the same one trained with Expert 1's annotations. This selection was necessary due to the significant disparity in the number of labels for less frequently represented classes (e.g., *Cholesteatoma* with 15 labels from E1 and 150 from E2).

- Normal Condition: The model achieves an F1 of 0.95 against E1 and 0.90 against E2, demonstrating good precision-recall balance compared to the inter-observer F1 of 0.92. This class presents high inter-operator agreement with (J = 0.85, Fig.3) that demonstrates such effectiveness by the experts.
- **Partial Obstruction:** F1 are 0.82 (E1) and 0.72 (E2). Despite a high inter-operator *J* of 0.87, this indicates a need for enhanced precision and potential confusion with similar conditions, as *Unlabelable* (J = 0.09, Fig.3).
- **Tympanosclerosis:** The model's F1 of 0.75 (E1) significantly surpasses the inter-observer F1 of 0.53, demonstrating improved detection capabilities. In contrast, the F1 drops to 0.50 when compared with E2, indicating a variability in detection accuracy across different experts. The observed disagreement between the two experts (J = 0.36, Fig.3) underscores the complexity of this task, particularly in efficiently detecting pathologies that may only slightly affect the tympanum's appearance.
- Earwax Plug: The model achieves an F1 of 0.75 when evaluated against E1's labels, which is below the inter-observer F1 of 0.87. It scores higher against E2, with an F1 of 0.90, with a perfect recall of 1. The software correctly detects the clearest cases of this pathology, similar to E2 who was more restrictive than E1 in his annotations.
- **Pseudotympanum:** Demonstrates an *F*1 of 0.58 (E1), but decreases to 0.18 on E2, which is in accordance with the low inter-observer F1 of 0.20. The low *J* of 0.11 for this condition underscores its complexity.

The F1 of the model against E2 is 0.82, indicating somewhat less optimal performance, which is normal as the model has been trained with E1 annotations. However, the decrease is not important considering the high inter-operator variability, demonstrating the robustness of the model.

So our model achieved a 91% accuracy rate across 5 classes (Table 6), incorporating a multilabel approach. Accuracy, in this context, refers to the proportion of correctly predicted instances among the total instances. This performance is comparable to bench-

Model	Fold 1	Fold 2	Fold 3	Fold 4	Fold 5	Mean (±SD)
ResNet50	0.83	0.83	0.85	0.84	0.83	0.84 (±0.01)
ResNet101	0.83	0.82	0.84	0.83	0.83	0.83 (±0.01)
VGG16	0.78	0.77	0.83	0.83	0.83	0.81 (±0.03)
VGG19	0.83	0.79	0.86	0.82	0.77	0.81 (±0.03)
DenseNet121	0.78	0.81	0.80	0.78	0.80	0.79 (±0.01)
DenseNet201	0.83	0.79	0.84	0.82	0.82	0.82 (±0.02)

Table 2: Jaccard scores of various models across five folds with their mean and standard deviation.

Table 3: ResNet50 classification metrics for otoscopy images using E1's labels on the test dataset. L_F indicates mean label count in each fold. Optimizing thresholds can lead to an improvement of up to 2 points in the sample average score.

Label	р	r	F1	L_F
Ventilation Tube	1.00	0.67	0.80	3
Earwax Plug	0.83	0.68	0.75	22
Mastoid Cavity	0.64	0.64	0.64	11
Cholesteatoma	0.50	1.00	0.67	1
Foreign Body	1.00	1.00	1.00	1
Unlabelable	0.50	0.50	0.50	2
Normal	0.94	0.95	0.95	374
Partial Obstruction	0.78	0.86	0.82	131
Osteomas	1.00	0.07	0.12	15
Atelectatic Otitis	1.00	0.27	0.42	15
External Otitis	1.00	0.67	0.80	6
Serous Otitis Media	0.67	1.00	0.80	4
Acute Middle Otitis	1.00	1.00	1.00	2
Otorrhea	0.80	0.80	0.80	5
Tympanic Perforation	0.60	0.55	0.57	11
Pseudotympanum	0.50	0.70	0.58	20
Stenosis	1.00	0.50	0.67	4
Tympanosclerosis	0.72	0.80	0.75	104
Samples Avg	0.88	0.88	0.88	731

marks set in other studies, which include 92.1% accuracy using InceptionResnet-v2 across 3 classes (Cha et al., 2019), 95.59% with DenseNet for 8 classes (Zeng et al., 2021), 97.47% with MobileNet for 3 classes (Wu et al., 2020), 84.4% with a custom CNN for 3 classes (Livingstone et al., 2019), and 91% with DenseNet for a single class (Habib et al., 2023a). This underscores the efficacy of our approach in handling complex multiclass scenarios.

4 CONCLUSION AND FUTURE WORKS

Our study validates the ResNet50 CNN's effectiveness in multi-label otoscopy image classification, Table 4: Classification metrics for otoscopy images, comparing E2's annotations with E1's labels. L denotes label support.

Label	р	r	F1	L
Ventilation Tube	1.00	1.00	1.00	32
Earwax Plug	0.98	0.78	0.87	228
Mastoid Cavity	0.69	0.77	0.73	35
Cholesteatoma	0.05	0.47	0.08	15
Foreign Body	0.78	1.00	0.88	7
Unlabelable	0.09	1.00	0.16	18
Normal	0.97	0.87	0.92	3795
Partial Obstruction	0.96	0.90	0.93	1233
Osteomas	0.79	0.80	0.80	173
Atelectatic Otitis	0.57	0.41	0.48	114
External Otitis	0.71	0.31	0.43	64
Serous Otitis Media	0.67	0.03	0.05	71
Acute Middle Otitis	0.40	0.23	0.29	26
Otorrhea	0.69	0.59	0.64	46
Tympanic Perforation	0.86	0.54	0.66	100
Pseudotympanum	0.45	0.13	0.20	209
Stenosis	0.33	0.10	0.16	29
Tympanosclerosis	0.95	0.36	0.53	1088
Samples Avg	0.89	0.80	0.83	7283

Table 5: ResNet50 classification metrics for otoscopy images, focusing on the most represented labels (with more than 200 items present in the dataset) using E2's labels on the test dataset. L_F indicates mean label count in each fold.

Label	р	r	F1	L_F
Earwax Plug	0.82	1.00	0.90	9
Normal	0.84	0.95	0.90	359
Partial Obstruction	0.88	0.61	0.72	140
Pseudotympanum	0.13	0.29	0.18	7
Tympanosclerosis	0.50	0.69	0.58	77
Samples Avg	0.80	0.83	0.82	637

achieving a notable F1 of 0.88 against first expert, and 0.82 against second expert. This indicates its high accuracy in identifying various ear conditions simultaneously. Our approach advances beyond traditional single-condition diagnostics, offering a more compre-

Га	b	le	6:	Accuracy	scores	for	main	represented	d la	bels	s.
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Label	Accuracy
Ear Wax	0.99
Normal	0.84
Partial Obstruction	0.85
Pseudotympanum	0.98
Tympanosclerosis	0.87
Mean	0.91

hensive multi-label analysis.

We plan to enhance our model by expanding our dataset to include a wider range of conditions, especially rare ones, improving robustness and diagnostic accuracy. Additionally, we will adopt a multimodal approach, integrating tonal and vocal audiometry with endoscopy imaging to enhance diagnostic precision. We also aim to leverage advanced vision language models like LLaMA to boost our classification performance. These developments are expected to significantly advance patient outcomes in clinical settings.

5 COMPLIANCE WITH ETHICAL STANDARDS

This study was conducted in accordance with the principles outlined in the Declaration of Helsinki. Informed consent was obtained from all individual participants involved in the study. Additionally, all patient data were collected in the current clinical pratice without modifying the patient's treatment pathway. To date, no study suggests that a photo of an eardrum or a earcanal can be used to identify a patient. Taken together, this data does not fall within the CNIL's definition of paersonal sensitive data. The data were anonymized to ensure privacy and confidentiality. Prior to their treatment, patients have given their consent for their data to be processed electronically and used anonymously for clinical and scientific studies, in accordance with general data protection regulations.

REFERENCES

- Cha, D., Pae, C., Seong, S., Choi, J., and Park, H. (2019). Automated diagnosis of ear disease using ensemble deep learning with a big otoendoscopy image database.
- Chen, Y.-C., Chu, Y.-C., Huang, C.-Y., Lee, Y.-T., Lee, W.-Y., Hsu, C.-Y., Yang, A. C., Liao, W.-H., and Cheng, Y.-F. (2022). Smartphone-based artificial intelligence using a transfer learning algorithm for the detection

and diagnosis of middle ear diseases: A retrospective deep learning study.

- Davis, J. and Goadrich, M. (2006). The relationship between precision-recall and roc curves. pages 233–240.
- Gulshan, V., Peng, L., and et al., M. C. (2016). Development and validation of a deep learning algorithm for detection of diabetic retinopathy in retinal fundus photographs. *JAMA*, 316(22):2402–2410.
- Habib, A., Xu, Y., Bock, K., et al. (2023a). Evaluating the generalizability of deep learning image classification algorithms to detect middle ear disease using otoscopy. *Scientific Reports*, 13:5368.
- Habib, A.-R., Xu, Y., Bock, K., Mohanty, S., Sederholm, T., Weeks, W. B., Dodhia, R., Ferres, J. L., Perry, C., Sacks, R., and Singh, N. (2023b). Evaluating the generalizability of deep learning image classification algorithms to detect middle ear disease using otoscopy. *Scientific Reports*, 13(1):5368.
- He, K., Zhang, X., Ren, S., and Sun, J. (2016). Deep residual learning for image recognition. pages 770–778.
- Huang, G., Liu, Z., van der Maaten, L., and Weinberger, K. Q. (2017). Densely connected convolutional networks. *Journal of Neural Networks*.
- Kingma, D. P. and Ba, J. (2015). Adam: A method for stochastic optimization.
- Kohavi, R. (1995). A study of cross-validation and bootstrap for accuracy estimation and model selection. 14(2):1137–1145.
- LeCun, Y., Bengio, Y., and Hinton, G. (2015). Deep learning. *Nature*, 521(7553):436–444.
- Livingstone, D., Talai, A. S., Chau, J., and Forkert, N. D. (2019). Building an otoscopic screening prototype tool using deep learning. *Journal of Otolaryngology Head & Neck Surgery*, 48(66). Published: 26 November 2019. Accesses: 3521, Citations: 27, Altmetric: 1.
- Olson, D. and Delen, D. (2008). Advanced data mining techniques.
- Shorten, C. and Khoshgoftaar, T. M. (2019). A survey on image data augmentation for deep learning. *Journal* of Big Data, 6(1):Article 60.
- Simonyan, K. and Zisserman, A. (2014). Very deep convolutional networks for large-scale image recognition. arXiv preprint arXiv:1409.1556.
- Viscaino, M., Maass, J., Delano, P., Torrente, M., Stott, C., et al. (2020). Computer-aided diagnosis of external and middle ear conditions: A machine learning approach. *PLOS ONE*, 15(3):e0229226.
- Wu, Z., Lin, Z., Li, L., Pan, H., Chen, G., Fu, Y., and Qiu, Q. (2020). Deep learning for classification of pediatric otitis media. *Pediatrics*. First published: 28 December 2020. Editor's Note: This Manuscript was accepted for publication on November 23, 2020. The authors have no funding, financial relationships, or conflicts of interest to disclose.
- Zeng, X., Jiang, Z., and et al., W. L. (2021). Efficient and accurate identification of ear diseases using an ensemble deep learning model.
- Zhou, Z., Huang, H., and Fang, B. (2021). Application of weighted cross-entropy loss function in intrusion detection. *Journal of Computer and Communications*, 9(11):1.