EMG-Based Shared Control Framework for Human-Robot Co-Manipulation Tasks

Francesca Patriarca^{Da}, Paolo Di Lillo^{Db} and Filippo Arrichiello^{Dc}

Department of Electrical and Information Engineering, University of Cassino and Southern Lazio, Via G. Di Biasio 43, 03043 Cassino (FR), Italy {francesca.patriarca1, pa.dilillo, filippo.arrichiello}@unicas.it

Keywords: Physical Human-Robot Interaction, Human-Robot Collaboration, Shared Control.

Abstract: The paper presents a shared control architecture designed for human-robot co-manipulation tasks, that allows the human to switch among robot's operational modes through surface electromyography (sEMG) signals from the user's arm. A support vector machine (SVM) classifier is employed to process the raw EMG data to identify two classes of contractions that are fed into a finite state machine algorithm to trigger the activation of different sets of admittance control parameters corresponding to the envisaged operational modes. The proposed architecture has been experimentally validated using a Kinova Jaco² manipulator, equipped with Force/Torque sensor at the end-effector, and with a user wearing Delsys Trigno Avanti EMG sensors on the dominant upper limb.

1 INTRODUCTION

Collaborative robotics involves robotic systems interacting directly with humans in a shared workspace to complete tasks together, combining the versatility and decision-making capabilities of human workers with the precision, strength, and repeatability of robots and improving task quality and productivity. Intuitive user interfaces, advanced sensors, and control systems are crucial for smooth cooperation and safe operation close to humans (Villani et al., 2018). Unlike industrial robots, collaborative robots (cobots) dynamically adapt to people and objects that enter their workspace (Matheson et al., 2019), without the need for physical barriers, making them suitable for various applications like logistics, assembly, and medical procedures (Sladić et al., 2021). However, developing effective human-robot teams presents challenges such as robots situational awareness, clear communication protocols, and ensuring safety without limiting robot's speed or motion (Sharifi et al., 2022). To address these challenges, shared control, which involves both the robot and the human as active parts in the control loop (Abbink et al., 2018), has emerged as a promising solution in collaborative robotics by enabling smoother interactions and im-



Figure 1: The scenario shows the experimental setup in which a human operator performs a co-manipulation task wearing four EMG sensors and using a Jaco² manipulator.

proving task efficiency and safety. To achieve this, impedance/admittance control strategies can be employed for controlling robots to behave as virtual dynamic systems with adjustable impedance parameters (Cacace et al., 2019). This allows the robot to adapt its compliance and motion synchronization capabilities to better interact with their environment (Fi-

46

Patriarca, F., Di Lillo, P. and Arrichiello, F. EMG-Based Shared Control Framework for Human-Robot Co-Manipulation Tasks. DOI: 10.5220/0012943600003822 Paper published under CC license (CC BY-NC-ND 4.0) In *Proceedings of the 21st International Conference on Informatics in Control, Automation and Robotics (ICINCO 2024) - Volume 2*, pages 46-53 ISBN: 978-989-758-717-7; ISSN: 2184-2809 Proceedings Copyright © 2024 by SCITEPRESS – Science and Technology Publications, Lda.

^a https://orcid.org/0009-0005-5849-6162

^b https://orcid.org/0000-0003-2083-1883

^c https://orcid.org/0000-0001-9750-8289

cuciello et al., 2015). The rates of change of interaction force and human arm admittance parameters can be used to modify the variable admittance parameters (Wang and Zhao, 2023); while predicting human motion trajectories enables robots to anticipate movements and adapt accordingly, optimizing task completion (Losey and O'Malley, 2018). In order to estimate user movement intentions, surface electromyography (sEMG) sensors, which capture muscle electrical activity, are essential (Grafakos et al., 2016). These sensors help to adapt virtual online damping, leading to the integration of EMG signals with adaptive admittance control in robotic manipulation, skill learning, and rehabilitation devices (Gonzalez-Mendoza et al., 2022). Integration of human motion prediction, adaptation algorithms, and virtual guidance also enhances the quality of assistance (Li et al., 2022), as demonstrated in applications like exoskeleton control (Zhuang et al., 2021). Furthermore, the sEMG signals also play a crucial role in encoding stiffness and movement patterns to improve robotic skill learning and adaptive behavior (Zeng et al., 2021).

This paper presents a shared control architecture for human-robot co-manipulation tasks that allows the human operator to dynamically change the robot's operational mode using sEMG signals from the user's arm and hand. These signals are classified by a Support Vector Machine (SVM) (Hearst et al., 1998) algorithm, which detects various contractions and movements. The output of the classifier is then fed into a finite state machine algorithm, which adjusts the parameters of a variable admittance controller to allow for better human-robot interaction. Since the dynamic behavior of the manipulator is not unique, managing different types of interactions in a unified way ensuring optimal co-manipulation experiences is not easy. Key factors in determining admittance parameters include the robot's compliance with forces applied by human, the fluidity and intuitiveness of the manual driving experience, and the speed and accuracy of task execution. Lower damping improves maneuverability but can cause instability or inaccuracy, while higher damping enhances precision but reduces compliance, making co-manipulation more difficult and slower. Using sEMG signals to adjust admittance parameters is a novel approach that ensures stable robot behavior, contrasting with previous methods relying on heuristics (Ferraguti et al., 2019) or specific stable region of parameters for specific interaction (Ficuciello et al., 2015). Wrench sensor readings make complex to distinguish intentional operator's gestures from unintentional collisions because the user holds the end-effector after the sensor that can not detect the forces between the contact

point and the environment if the forces are exerted by the user; while integrating musculoskeletal activity allows to recognize such interactions that would be indistinguishable otherwise.

The paper presents a shared control architecture that dynamically changes the variable admittance controller parameters based on the operator's EMG signals to enhance precision in task performance by reducing downtime, improving human-robot interactions for a more intuitive co-manipulation experience. The approach's effectiveness and robustness have been experimentally validated with a user wearing four sEMG sensors on his/her dominant upper limb and using a 7DOF manipulator equipped with a Force/Torque sensor for admittance control, despite not being torque-controlled.

2 SHARED CONTROL ARCHITECTURE

The proposed architecture includes two possible operational modes:

- *Low-Damping* mode: hand-guidance of the endeffector in the free space to allow the operator to move the end-effector, e.g., to reach a workpiece;
- *High-Damping* mode: hand-guidance of the endeffector near a surface or a workpiece to perform operations such as welding or painting.

To achieve this, the gains of the admittance controller of the manipulator are changed between two sets corresponding to each operational mode. A finite state machine algorithm handles the switching between these sets based on the movements or contractions of the operator's arm, which are recognized through an EMG-based classifier.

Figure 2 shows the block diagram of the entire shared control architecture. The High-level layer includes all the functional blocks that generate specific sets of admittance gains, while the Low-level layer includes all the blocks that concern the motion control of the manipulator. The raw EMG signals go as input to a SVM classifier that recognizes two possible classes of motions/contractions of the operator. The finite state machine algorithm receives this information and it sets the admittance gains based on the operational mode; then, an admittance controller (Di Lillo et al., 2021) outputs a desired trajectory for the endeffector, which is finally tracked by computing the needed joint velocity with an inverse kinematics algorithm (Di Lillo et al., 2023). In the following sections, details about all the functional blocks are given in a bottom-up order.



Figure 2: Proposed shared control architecture. The High-Level layer is responsible for the EMG signal acquisition and classification. Then, the recognized class is used into a finite-state machine algorithm that outputs a set of admittance gains. The Low-Level layer is responsible for the motion control of the manipulator, and it employs a variable admittance controller, an inverse kinematics algorithm and a joints controller.

3 LOW-LEVEL LAYER

The low-level layer implements the robot control algorithm and consists of three blocks: *i*) the joints controller, that generates actual joint velocity commands based on joint encoder readings and the inverse kinematics controller output; *ii*) the inverse kinematics controller, which computes the desired joint velocities that make the end-effector track the *desired* trajectory; and *iii*) the variable admittance controller, that modifies the input *reference* trajectory for the end-effector, using wrench sensor readings, to achieve a desired dynamic behavior, and outputs a new *desired* trajectory for the end-effector.

3.1 Inverse Kinematics and Joints Controller

Considering a serial manipulator with *n* Degrees of Freedom (DOFs), the state of the system is described by the vector $\boldsymbol{q} = [q_1, q_2, \cdots, q_n]^T \in \mathbb{R}^n$, which contains the joint positions. Define the vector that gathers the end-effector configuration as $\boldsymbol{x} = [\boldsymbol{p}^T \boldsymbol{o}^T]^T \in \mathbb{R}^7$, where $\boldsymbol{p} = [p_x, p_y, p_z]^T \in \mathbb{R}^3$ represents the coordinates of the end-effector expressed in the arm base frame, while $\boldsymbol{o} = [o_x, o_y, o_z, o_w]^T \in \mathbb{R}^4$ is the quaternion that expresses the orientation of the end-effector with respect to the arm base frame. The velocity of the end-effector can be described by the vector $\boldsymbol{v} = [\boldsymbol{p}^T \boldsymbol{\omega}^T]^T \in \mathbb{R}^6$, where $\boldsymbol{p} = [\dot{p}_x, \dot{p}_y, \dot{p}_z]^T \in \mathbb{R}^3$ and $\boldsymbol{\omega} = [\omega_x, \omega_y, \omega_z]^T \in \mathbb{R}^3$ represent the end-effector linear and angular velocities, respectively. The differential relationship between the end-effector velocity and the joint velocity vector $\boldsymbol{q} = [\dot{\boldsymbol{q}}_1, \dot{\boldsymbol{q}}_2, \cdots, \dot{\boldsymbol{q}}_n]^T$ can be expressed as $\boldsymbol{v} = \boldsymbol{J} \boldsymbol{\dot{q}}$, where $\boldsymbol{J} \in \mathbb{R}^{6 \times n}$ is the robot Jacobian matrix.

Assuming a redundant manipulator, i.e. n > 6, and the availability of a *desired* end-effector trajectory expressed as:

$$\boldsymbol{x}_{d} = \begin{bmatrix} \boldsymbol{p}_{d} \\ \boldsymbol{o}_{d} \end{bmatrix} \in \mathbb{R}^{7} \quad \boldsymbol{v}_{d} = \begin{bmatrix} \dot{\boldsymbol{p}}_{d} \\ \boldsymbol{\omega}_{d} \end{bmatrix} \in \mathbb{R}^{6} \quad \boldsymbol{a}_{d} = \begin{bmatrix} \ddot{\boldsymbol{p}}_{d} \\ \boldsymbol{\alpha}_{d} \end{bmatrix} \in \mathbb{R}^{6}$$
(1)

where x_d represents the desired position and quaternion, v_d gathers the desired linear and angular velocities and a_d represents the desired linear and angular accelerations. The desired joint velocity that makes the end-effector track the desired trajectory can be computed by resorting to the Closed-Loop Inverse Kinematics (CLIK) algorithm:

$$\dot{\boldsymbol{q}}_d = \boldsymbol{J}^{\dagger} (\boldsymbol{v}_d + \boldsymbol{K}_{\mathrm{ik}} \tilde{\boldsymbol{x}}) , \qquad (2)$$

where J^{\dagger} is the Moore-Penrose pseudoinverse of the Jacobian matrix, $K_{ik} \in \mathbb{R}^{6 \times 6}$ is a positive-definite matrix of gains and \tilde{x} is the error vector, defined as:

$$\tilde{\mathbf{x}} = \begin{bmatrix} \tilde{\mathbf{p}} \\ \tilde{\mathbf{o}} \end{bmatrix} = \begin{bmatrix} \mathbf{p}_d - \mathbf{p}(\mathbf{q}_d) \\ \mathbf{o}_d^{-1} \star \mathbf{o}(\mathbf{q}_d) \end{bmatrix} \in \mathbb{R}^6 , \qquad (3)$$

where \tilde{p} and \tilde{o} are the position and quaternion errors, respectively, q_d is the vector of desired joint position obtained by numerically integrating the desired joint velocity vector \dot{q}_d , $p(q_d)$ and $o(q_d)$ are the position and orientation of the end-effector obtained by considering q_d as joint positions in the direct kinematics computation.

Finally, the desired joint velocity vector is passed to the joints controller, which computes the actual command to send to the manipulator by resorting to a proportional controller including a feedforward action as:

$$\dot{\boldsymbol{q}}_r = \dot{\boldsymbol{q}}_d + \boldsymbol{K}_{\rm jc} \tilde{\boldsymbol{q}} , \qquad (4)$$

where $\mathbf{K}_{jc} \in \mathbb{R}^{n \times n}$ is a positive-definite matrix of gains and $\tilde{\mathbf{q}} = \mathbf{q}_d - \mathbf{q}$ is the joint position error computed with respect to the actual readings of the joint encoders.

3.2 Admittance Control

The admittance controller aims to assign a virtual dynamics to the manipulator, characterized by a desired mass, damping, and stiffness. More in detail, assuming to have a wrench sensor mounted on the wrist of the manipulator and to have a certain reference trajectory for the end-effector, the desired end-effector trajectory must have the following dynamics:

$$\boldsymbol{K}_m \, \tilde{\boldsymbol{a}}_{r,d} + \boldsymbol{K}_d \, \tilde{\boldsymbol{v}}_{r,d} + \boldsymbol{K}_k \, \tilde{\boldsymbol{x}}_{r,d} = \boldsymbol{h} \,, \tag{5}$$

where the positive-definite matrices:

$$\boldsymbol{K}_{m} = \begin{bmatrix} \boldsymbol{K}_{m}^{p} & \boldsymbol{O}_{3\times3} \\ \boldsymbol{O}_{3\times3} & \boldsymbol{K}_{m}^{o} \end{bmatrix}$$
(6)

$$\boldsymbol{K}_{d} = \begin{bmatrix} \boldsymbol{K}_{d}^{p} & \boldsymbol{O}_{3\times3} \\ \boldsymbol{O}_{3\times3} & \boldsymbol{K}_{d}^{o} \end{bmatrix}$$
(7)

$$\boldsymbol{K}_{k} = \begin{bmatrix} \boldsymbol{K}_{k}^{p} & \boldsymbol{O}_{3\times3} \\ \boldsymbol{O}_{3\times3} & \boldsymbol{K}_{k}^{o} \end{bmatrix}, \qquad (8)$$

represent the virtual mass, damping, and stiffness, respectively, where the position $K_{(.)}^p$ and orientation $\boldsymbol{K}_{(\cdot)}^{o}$ gains are highlighted, $\boldsymbol{h} = \left[\boldsymbol{f}^{\mathrm{T}} \boldsymbol{\mu}^{\mathrm{T}}\right]^{\mathrm{T}} \in \mathbb{R}^{6}$ is the vector stacking the linear force and moments measured by the wrench sensor, and:

$$\tilde{\boldsymbol{x}}_{r,d} = \begin{bmatrix} \tilde{\boldsymbol{p}}_{r,d} \\ \tilde{\boldsymbol{o}}_{r,d} \end{bmatrix} = \begin{bmatrix} \boldsymbol{p}_r - \boldsymbol{p}_d \\ \boldsymbol{o}_r^{-1} \star \boldsymbol{o}_d \end{bmatrix}$$
(9)
$$\tilde{\boldsymbol{v}}_{r,d} = \boldsymbol{v}_r - \boldsymbol{v}_d$$
(10)

$$= \boldsymbol{v}_r - \boldsymbol{v}_d \tag{10}$$

$$\tilde{\boldsymbol{a}}_{r,d} = \boldsymbol{a}_r - \boldsymbol{a}_d \;, \tag{11}$$

are the operational space configuration, velocity and acceleration errors computed between the reference and the desired trajectories. The desired acceleration in output from the admittance controller can be computed by folding Eqs (9)-(11) in Eq. (5) and rearranging the terms, obtaining:

$$\boldsymbol{a}_{d} = \boldsymbol{K}_{m}^{-1} \left[\boldsymbol{K}_{m} \, \boldsymbol{a}_{r} + \boldsymbol{K}_{d} \, \tilde{\boldsymbol{\nu}}_{r,d} + \boldsymbol{K}_{k} \, \tilde{\boldsymbol{x}}_{r,d} - \boldsymbol{h} \right] \,. \tag{12}$$

The desired end-effector velocity v_d and configuration \mathbf{x}_d to be tracked by the inverse kinematics controller in Eq. (2) can then be obtained by numerical integration of the desired acceleration. It is worth noticing that the virtual mass, damping and stiffness can be varied, obtaining a variable admittance controller.

Each one of the operational modes listed in Sec. 2 has a corresponding set of admittance gains that adjust the robot's behavior to successfully execute them. In detail, with reference to Eqs. (6)-(8), when in Low-*Damping* mode the K_k gain is set to $O_{6\times 6}$ to allow the operator to freely change the end-effector position and orientation. The matrix \mathbf{K}_d^p is set as $\mathbf{K}_d^p =$ diag{ $k_{d,\text{low}}^p, k_{d,\text{low}}^p, k_{d,\text{low}}^p$ }, with *low* element $k_{d,\text{low}}^p$ to assure smooth teleoperation to the user; similarly,

for the orientation, the matrix \mathbf{K}_d^o is set as $\mathbf{K}_d^o =$ diag{ $k_{d,\text{low}}^o, k_{d,\text{low}}^o, k_{d,\text{low}}^o$ }, with *low* element $k_{d,\text{low}}^o$. Regarding the virtual mass, the matrix \boldsymbol{K}_m^p is set to diag = { $k_{m,\text{low}}^p, k_{m,\text{low}}^p, k_{m,\text{low}}^p$ }, while the matrix \boldsymbol{K}_m^o is

set to diag = { $k_{m,low}^{p}$, $k_{m,low}^{p}$, $k_{m,low}^{o}$ }, $k_{m,low}^{o}$ }. When in *High-Damping* mode the \mathbf{K}_{k} gain is still set to $\mathbf{O}_{6\times 6}$, while \mathbf{K}_{d}^{p} is set as \mathbf{K}_{d}^{p} = diag{ $k_{d,high}^{p}$, $k_{d,high}^{p}$, $k_{d,high}^{p}$ } with *high* element $k_{d,high}^{p}$ to ensure slow and precise movements, for example when painting a thin element. Regarding the orientation, the matrix \mathbf{K}_{d}^{o} is set as $\mathbf{K}_{d}^{o} = \text{diag}\{k_{d,\text{high}}^{o}, k_{d,\text{high}}^{o}, k_{d,\text{high}}^{o}\}$, with *high* element $k_{d,\text{low}}^{o}$. Finally, the virtual mass, the matrix \mathbf{K}_{m}^{p} is set to diag = $\{k_{m,\text{high}}^{p}, k_{m,\text{high}}^{p}, k_{m,\text{high}}^{p}\}$, while the matrix \mathbf{K}_{m}^{o} is set to diag = $\{k_{m,\text{high}}^{o}, k_{m,\text{high}}^{o}, k_{m,\text{high}}^{o}, k_{m,\text{high}}^{o}\}$.

HIGH-LEVEL LAYER 4

The high-level layer is composed of three main functional blocks: i) the EMG sensors, ii) the operator's motion classifier, and iii) the finite state machine algorithm.

EMG Signal Analysis 4.1

Electromyography (EMG) signals, produced by muscle contractions and relaxations, are detected using surface or needle-based electrodes, and need to be amplified and filtered to remove noise. In this works EMG signals are used to detect muscle activity and patterns. The proposed solution refers to a Support Vector Machine classifier, a common supervised learning algorithm for classification tasks, that processes features extracted from EMG signals segmented into time windows (or epochs), specifically using three commonly time-domain features: Root Mean Square (RMS), Mean Absolute Value (MAV) and Average Amplitude Change (AAC) (Li et al., 2022).

To train the SVM classifier, a dataset of feature vectors with associated class labels, obtained with a predetermined acquisition procedure, is used. The SVM algorithm learns a decision boundary to separate different classes by finding an optimal hyperplane in the feature space, governed by two main hyperparameters: the regularization parameter C, which prevents overfitting by limiting misclassification, and γ , which determines how much far points influence the hyperplane calculation. During the training, the SVM adjusts the parameters by solving a quadratic programming problem to identify the support vectors, i.e., the points closest to the decision boundary.

In the proposed scenario, the classifier is trained to discriminate between two classes: *free* (movements made by the operator in various directions with minimal resistance) and *contraction* (generated by the operator by tightening his hand).

4.2 Finite State Machine

The two classes in output from the SVM classifier are fed into a finite state machine algorithm to automatically switch between the operational modes, as shown in Figure 3.



Figure 3: Finite State Machine.

In detail, the system starts in *Low-Damping* mode; when the operator executes the *contraction* class for at least 1.5s, the state switches to *High-Damping* mode, corresponding to a set of admittance gains that allow the operator to move the end-effector to follow a predefined path, without touching it, with lower speed and higher accuracy due to the increased damping. By generating the *contraction* class for at least 3s, the state returns to the *Low-Damping* mode, in which the operator can move the end-effector more easily and faster towards the starting point to execute the path again.

5 EXPERIMENTAL VALIDATION

5.1 Experimental Setup

To validate the effectiveness of the proposed shared control architecture, experiments of human-robot comanipulation tasks were conducted using a 7DOF Kinova Jaco² manipulator¹ equipped with a Bota Systems Rokubimini force/torque sensor². Four noninvasive Delsys Trigno Avanti active sensors³ with a frequency of 1.78 kHz were placed on the dominant arm of the human operator. Following Seniam guidelines⁴, they were put on the *biceps* and *triceps brachii*, *flexor carpi radialis* and *extensor carpi ulnaris* muscles, as much as possible in the center of muscles. The streaming of EMG data was done through a Python GUI on a Windows PC, while the control software and the SVM classifier, developed using Python and the Scikit-learn library (Kramer, 2016), were implemented in the ROS (Robotic Operating System) framework running on Linux. To allow the two workstations to communicate TCP/IP sockets were used.

5.2 Training and Test of the Classifier

To train the SVM classifier described in section 4.1, EMG signals from a human operator's arm were recorded while performing specific movements or contractions interacting with a manipulator. Two interactions were considered for data collection: in the first, the robot's behavior was made compliant, using the Low-Damping mode parameters, and the operator moved the end-effector in random directions to collect data related to the *free* class; in the second, the robot had a rigid behavior, obtained by referring to a standard position controller, and the operator tightened the hand on the end-effector handle to collect data related to the contraction class. A Matlab GUI told the operator which movements or contractions to perform and automatically labeled the data to obtain two datasets: one for training and one for testing the classifier. For each of the four EMG sensors, three time-domain features were extracted, resulting in a 12-element feature vector, with an associated class label. The SVM model is trained using the hyperparameters in Table 1. The confusion matrix for binary problems, where the rows represent the expected class distribution and the columns the predicted distribution by the classifier, was used to evaluate classifier performance and to compute class metrics such as Accuracy, Precision, Recall, and F1-score, yielding the following indexes:

$$A = \frac{TP}{TP + TN + FP + FN} \qquad P = \frac{TP}{TP + FP}$$
$$R = \frac{TP}{TP + FN} \qquad F1 = \frac{TP}{TP + \frac{FN + FP}{2}}$$

where TP, TN, FP and FN are true positives/negatives and false positives/negatives taken from the binary problem confusion matrix, respectively. True positives and negatives are the correctly

¹https://www.kinovarobotics.com/product/gen2-robots

²https://www.botasys.com/force-torque-sensors/rokubi ³https://delsys.com/trigno-avanti/. These sensors have an integrated pre-amplification circuit to reduce input noise

and do not require amplifying and filtering signals.

⁴http://seniam.org

identified positive/negative classes, while false positives and negatives are the incorrectly classified values. The accuracy measures how many instances were correctly classified, the precision measures the accuracy of the positive predictions, the recall is the ratio of positive instances that are correctly detected, and the F1-score is the harmonic mean of precision and recall.

In the on-line use of the classifier, the statistical mode of the predicted classes calculated over the last 1.5s is sent to the finite state machine to increase the robustness in terms of misclassifications.

5.3 Experimental Results

To validate the overall architecture by triggering all the envisioned state transitions, a series of experiments were performed in which a subject⁵ (female, aged 29) wearing EMG sensors had to guide the robot end-effector several times along a predefined path, as if she were performing a painting operation on a thin element, as shown in Figure 1. The path consists of a cylindrical filament whose shape is similar to a square wave. The user repeated the designed experiment 15 times to test the reproducibility of the approach.

Table 1: Experimental parameters used in the proposed architecture.

Control parameters					
Parameter	Value	Value Description			
K _{ik}	diag{20 I ₃ , 15 I ₃ }	Inverse kinematics gain			
$\boldsymbol{K}_{\mathrm{jc}}$	diag $\{3 I_4, 2 I_3\}$	Joints controller gain			
$k_{d,\text{low}}^p$	40	Low-damping position gain			
$k_{d,\text{low}}^{o}$	2	Low-damping orientation gain			
$k_{m,\text{low}}^p$	3	Low-mass position gain			
$k_{m,\text{low}}^{o}$	0.1	Low-mass orientation gain			
$k_{d,\text{high}}^p$	120	High-damping position gain			
$k_{d, high}^{o}$	4	High-damping orientation gain			
$k_{m, high}^p$	5	High-mass position gain			
$k^o_{m, { m high}}$	0.1	High-mass orientation gain			
Classifier parameters					
Parameter	Value	Description			
С	1	Regularization parameter			
γ	'scale' ⁶	Parameter of a Gaussian Kernel			
Kernel	'RBF'	Kernel used in the SVM Classifier			

⁵The experiments were taken in accordance with the Declaration of Helsinki, the protocol has been approved by the Research Ethics Committee at the university where the study is conducted and the subject gave informed consent.

Table 1 shows the parameters for the controllers and the classifier used in the experiments, where all the admittance parameters were experimentally determined; while a video showing the experiments is provided at the following link: https://youtu.be/93u5i8HmsPY.



Figure 4: The confusion matrix obtained after training the classifier.

In the following, the results of the classifier performances and the experimental execution are discussed. In particular, the confusion matrix is shown in Figure 4, while Table 2 contains the classifier indexes. All performance indexes exceed 99%, as indicated in the confusion matrix, which has only 1.8% of misclassifications for *contraction* class. This means that, in addition to the high classification performance attested by the high accuracy value, the number of false positives is also very low. The precision and recall also indicate a solid balance confirmed by the F1score, whose value is close to the accuracy. Thus, the numerical results attest a reliable and accurate classification capability, also supported by the use of only two classes.

Table 2: Table containing performance evaluation metrics.

Accuracy (%)	Precision (%)	Recall (%)	F1-Score (%)
99.20	99.28	99.12	99.19

Figure 5 shows the path followed by the endeffector during one of the experiments performed, including the start and end points. Two different colors were used to highlight the path followed by the manipulator, depending on the corresponding active operational mode: green and blue paths correspond to Low-Damping and High-Damping modes, respectively. The user drives the end-effector near the beginning of the filament to be followed, generates the contraction class for 1.5s to switch to High-Damping mode, and moves the end-effector along the filament without touching it using the free class. By generating contraction for at least 3s, the user switches the FSM back to Low-Damping mode and quickly moves the end-effector back to start point with the free class (as can be seen by the green edge connecting the ends of the blue lines). Then, the user generates contrac-

⁶'scale' is a parameter calculated as 1 divided by the product of the features number and the variance of the feature vector.

tion for 1.5s, returning the FSM to *High-Damping* mode, and uses the *free* class to follow the filament again; in fact, there are two blue lines in the shape of a square wave. Finally, the user switches the FSM back to *Low-Damping* mode using *contraction* for 3s and moves the manipulator to the endpoint.



Figure 5: The path followed by the manipulator's endeffector in one of the experiments performed. The path is highlighted with two colors based on the two operational modes: *Low-Damping* mode is marked in green and *High-Damping* mode is highlighted in blue.

The user was able to complete the experiment without difficulty by easily changing the operational modes, as outlined in the NASA-TLX questionnaire she completed.

Figure 6 shows the time evolution of the classifier output, the force measured by the F/T sensor, and the linear velocity of the manipulator's end-effector. Similarly to what was highlighted in the performed path, the colors green and blue indicate the Low-Damping and High-Damping modes, respectively. In particular, Figure 6a shows the time evolution of the classifier output, which provides information about how it was able to distinguish between free and contraction classes. The classifier output determines the transition between the control modes, as highlighted by the different colored areas; in fact, after the first 6s (or after 83s) in which the operator is in free class, she generates contraction for 1.5s and the FSM switches to High-Damping mode; the FSM remains in the same state until the operator stops following the filament; then, the operator generates a 3s contraction (after 72 or 146s) and the FSM returns to Low-Damping mode. Instead, the time evolution of the force and linear velocity of the end-effector are shown in Figures 6b and 6c, respectively. The velocity increases significantly in the green areas, corresponding to a mode with low damping values, compared to the blue areas where, since the damping is higher, the manipulator becomes less compliant and moves more slowly during the comanipulation.



Figure 6: Experimental results: a) EMG Classifier Output; b) Force measured by the F/T sensor; c) End-Effector Linear Velocity. The different colored areas on all graphs correspond to the two different control modes: green and blue represent the *Low-Damping* and the *High-Damping* modes, respectively.

Oscillations in the force trend also increase in the green areas corresponding to *Low-Damping*, especially when the user generates the *contraction* class to switch modes. In the transition from *Low-Damping* to *High-Damping* this happens because, before the transition occurs, the force sensor perceives the user's hand as a rigid external environment; while in the transition from *High-Damping* to *Low-Damping* the operator does not stop contracting immediately after the transition because of his reflexes, and the lower damping is not sufficient to reduce the oscillations due to residual contractions.

6 CONCLUSIONS

In this work, a shared control architecture is proposed that allows changing the admittance parameters of a manipulator using sEMG sensors in a human-robot co-manipulation scenario. A dedicated classifier recognizes the human movements and contractions to switch among two sets of admittance parameters corresponding to two robot behaviors. The robustness of the approach is validated using a Jaco² manipulator and four Trigno Avanti EMG sensors through a series of experiments. The interaction with external environment can produce oscillations that can cause resonance phenomena (known in the literature), especially when the robot comes into contact with more rigid environments. Future work will be devoted to analyze these phenomena in order to extend this approach to more complex scenarios where both humanrobot and robot-environment interactions are considered. This will require an increase in the number of operational modes to handle complex scenarios and, consequently, the introduction of a greater number of classes from EMG signals.

ACKNOWLEDGEMENTS

The research leading to these results has received funding from Project *COM*³ CUP H53D23000610006 funded by EU in NextGenerationEU plan through the Italian "Bando Prin 2022 - D.D. 104 del 02-02-2022" by MUR, from H2020-ICT project CANOPIES (Grant Agreement N. 101016906), and by Project "Ecosistema dell'innovazione - Rome Technopole" financed by EU in NextGenerationEU plan through MUR Decree n. 1051 23.06.2022.

REFERENCES

- Abbink, D. A., Carlson, T., Mulder, M., de Winter, J. C. F., Aminravan, F., Gibo, T. L., and Boer, E. R. (2018). A topology of shared control systems—finding common ground in diversity. *IEEE Transactions on Human-Machine Systems*, 48(5):509–525.
- Cacace, J., Caccavale, R., Finzi, A., and Lippiello, V. (2019). Variable admittance control based on virtual fixtures for human-robot co-manipulation. In 2019 IEEE International Conference on Systems, Man and Cybernetics (SMC), pages 1569–1574.
- Di Lillo, P., Simetti, E., Wanderlingh, F., Casalino, G., and Antonelli, G. (2021). Underwater intervention with remote supervision via satellite communication: Developed control architecture and experimental results within the dexrov project. *IEEE Transactions on Control Systems Technology*, 29(1):108–123.
- Di Lillo, P., Vito, D. D., and Antonelli, G. (2023). Merging global and local planners: Real-time replanning algorithm of redundant robots within a task-priority framework. *IEEE Transactions on Automation Science and Engineering*, 20(2):1180–1193.
- Ferraguti, F., Talignani Landi, C., Sabattini, L., Bonfe, M., Fantuzzi, C., and Secchi, C. (2019). A variable admittance control strategy for stable physical human–robot interaction. *The International Journal of Robotics Research*, 38(6):747–765.
- Ficuciello, F., Villani, L., and Siciliano, B. (2015). Variable impedance control of redundant manipulators for intuitive human–robot physical interaction. *IEEE Transactions on Robotics*, 31(4):850–863.

- Gonzalez-Mendoza, A., Quinones-Uriostegui, I., Salazar-Cruz, S., Perez Sanpablo, A. I., López, R., and Lozano, R. (2022). Design and implementation of a rehabilitation upper-limb exoskeleton robot controlled by cognitive and physical interfaces. *Journal of Bionic Engineering*, 19.
- Grafakos, S., Dimeas, F., and Aspragathos, N. (2016). Variable admittance control in pHRI using EMG-based arm muscles co-activation. In 2016 IEEE International Conference on Systems, Man, and Cybernetics (SMC), pages 001900–001905.
- Hearst, M. A., Dumais, S. T., Osuna, E., Platt, J., and Scholkopf, B. (1998). Support vector machines. *IEEE Intelligent Systems and their applications*, 13(4):18– 28.
- Kramer, O. (2016). Scikit-learn. Machine learning for evolution strategies, pages 45–53.
- Li, J., Li, G., Chen, Z., and Li, J. (2022). A novel emgbased variable impedance control method for a teleoperation system under an unstructured environment. *IEEE Access*, 10:89509–89518.
- Losey, D. P. and O'Malley, M. K. (2018). Trajectory deformations from physical human–robot interaction. *IEEE Transactions on Robotics*, 34(1):126–138.
- Matheson, E., Minto, R., Zampieri, E. G. G., Faccio, M., and Rosati, G. (2019). Human–robot collaboration in manufacturing applications: A review. *Robotics*, 8(4).
- Sharifi, M., Zakerimanesh, A., Mehr, J. K., Torabi, A., Mushahwar, V. K., and Tavakoli, M. (2022). Impedance variation and learning strategies in human-robot interaction. *IEEE Transactions on Cybernetics*, 52(7):6462–6475.
- Sladić, S., Lisjak, R., Runko Luttenberger, L., and Musa, M. (2021). Trends and progress in collaborative robot applications. *Politehnika*, 5:32–37.
- Villani, V., Pini, F., Leali, F., and Secchi, C. (2018). Survey on human–robot collaboration in industrial settings: Safety, intuitive interfaces and applications. *Mechatronics*, 55:248–266.
- Wang, C. and Zhao, J. (2023). Based on human-like variable admittance control for human-robot collaborative motion. *Robotica*, 41(7):2155–2176.
- Zeng, C., Yang, C., Cheng, H., Li, Y., and Dai, S.-L. (2021). Simultaneously encoding movement and sEMG-based stiffness for robotic skill learning. *IEEE Transactions on Industrial Informatics*, 17(2):1244– 1252.
- Zhuang, Y., Leng, Y., Zhou, J., Song, R., Li, L., and Su, S. W. (2021). Voluntary control of an ankle joint exoskeleton by able-bodied individuals and stroke survivors using emg-based admittance control scheme. *IEEE Transactions on Biomedical Engineering*, 68(2):695–705.